

Graph-based learning in medical imaging and imaging genetics

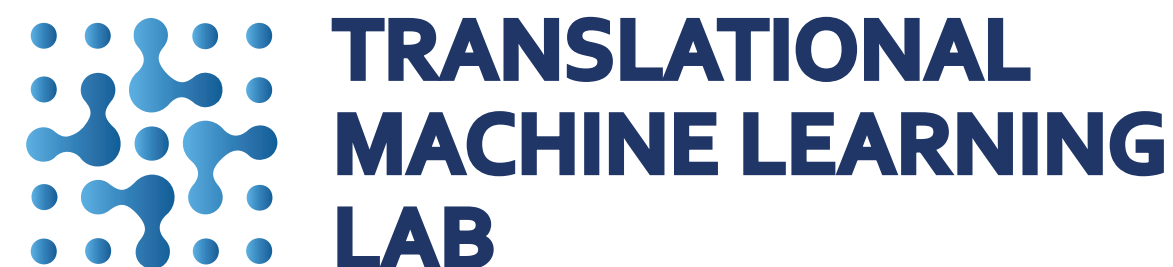
Jonas Richiardi



@TranslationalML



<https://unil.ch/tml>



Agenda

Background and motivation: why graphs ?

Graph estimation: from images to graphs

Graph analysis: from graphs to models and inference

Graph imaging genetics: using graphs as endophenotypes

1. Background & motivation

Medical imaging data

2D

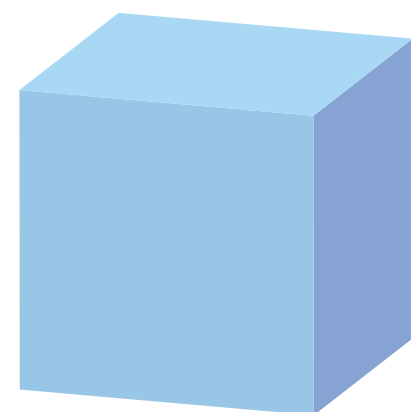


Radiograph

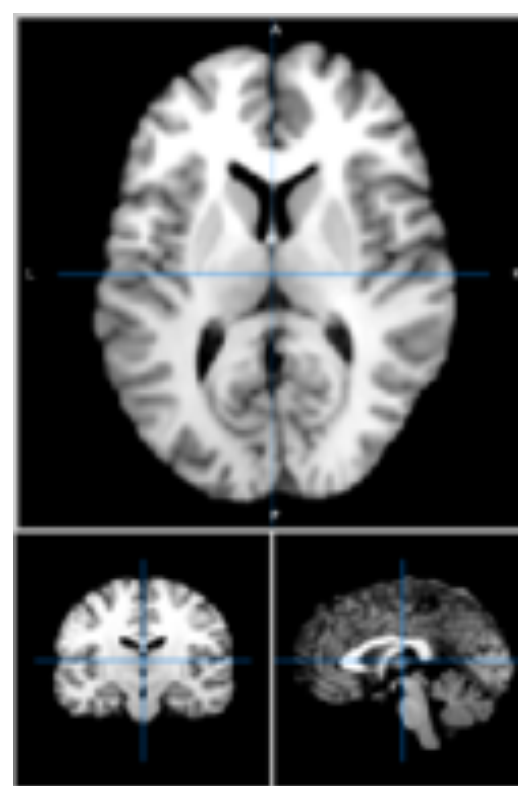


1500x2000

3D

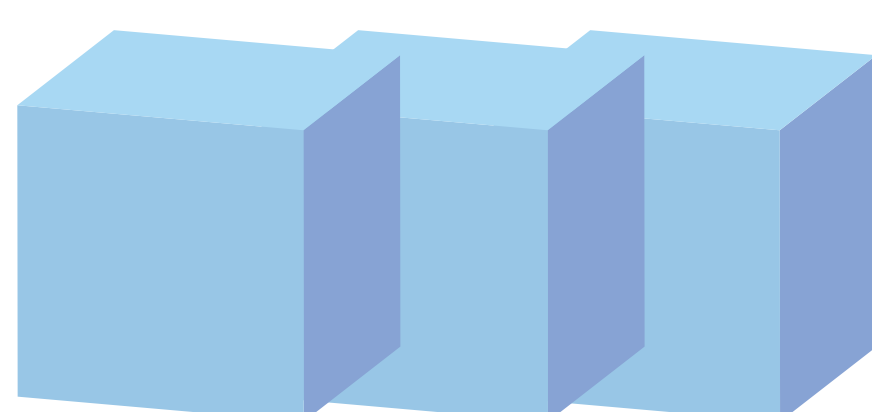


T1w sMRI

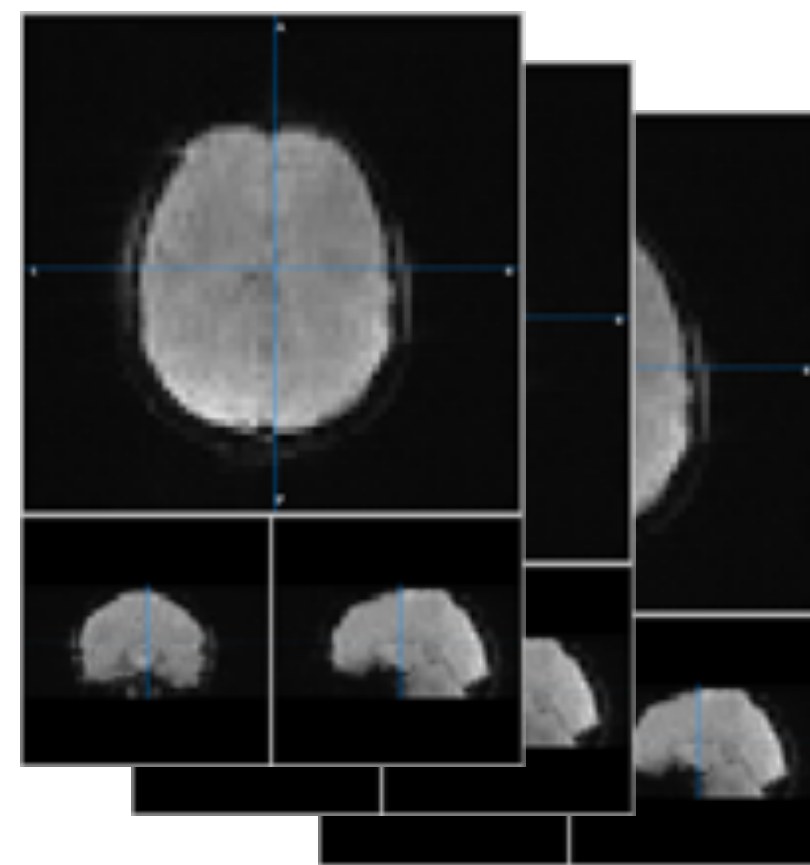


161x191x151

4D



BOLD fMRI

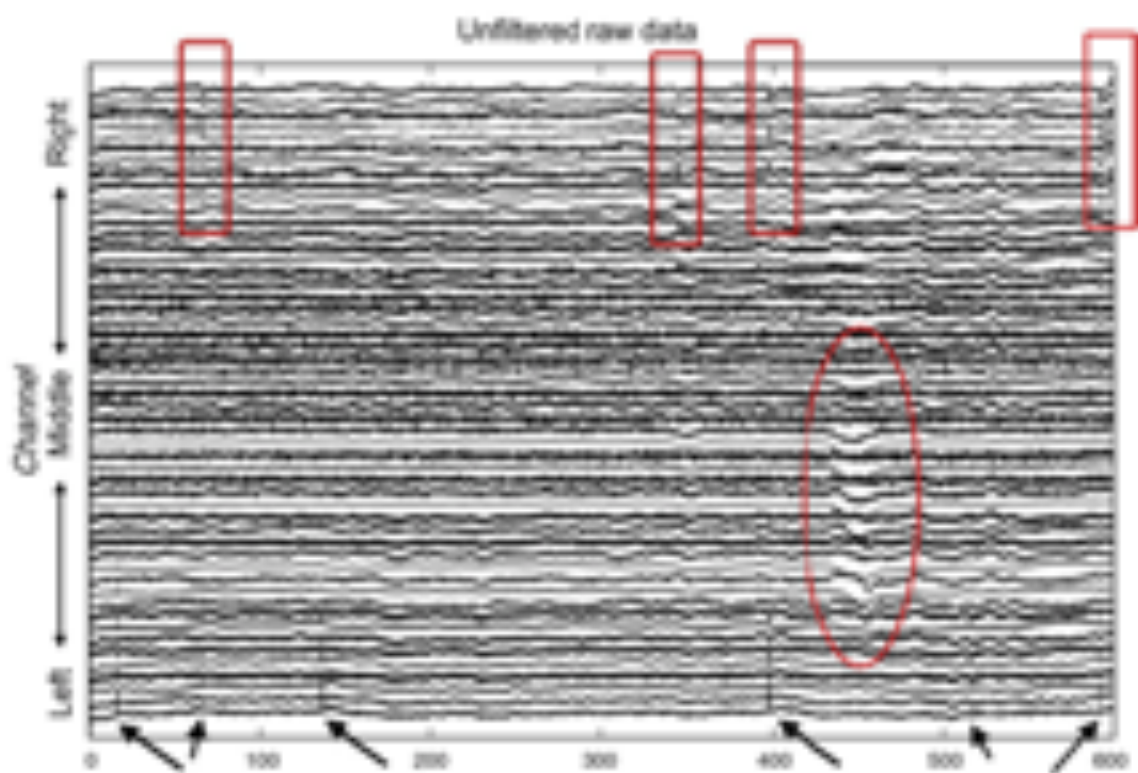


64x61x21@0.9 Hz

MVTS



fNIRS



52x600@10Hz

What types of analyses can we perform?

Image → Image prediction

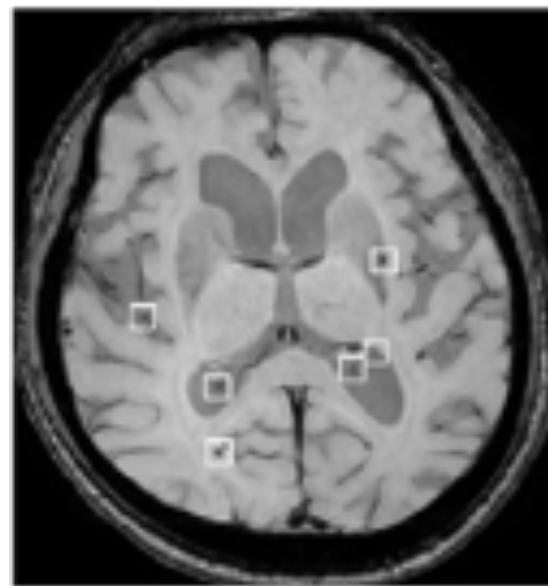
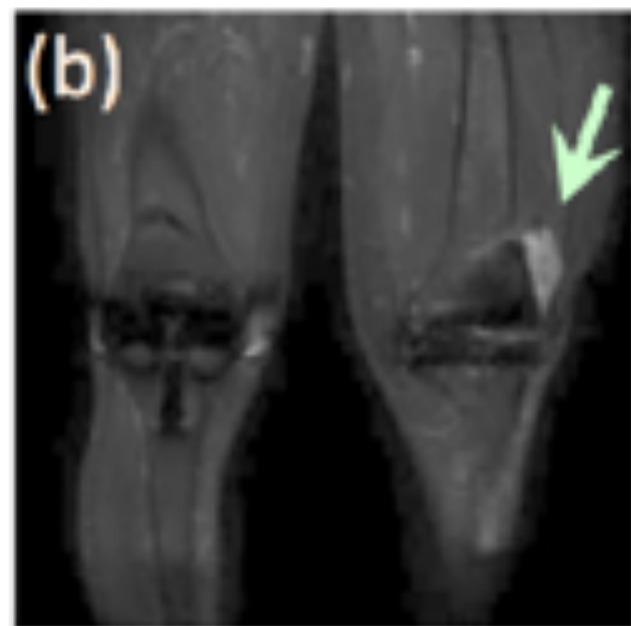


Image (+X) → Clinical prediction



label: abscess

abscess: 0.663
infection: 0.103
osteochondromatosis: 0.037
synovitis: 0.032
cyst: 0.026



Acquisition/Reconstruction/Image processing

I→I Synthetic contrast generation

I→I Multi-site data

S→I Sequence/Reconstruction optimisation (RF pulse design)



Diagnosis

I→I: lesion segmentation, abnormality detection (e.g. Aneurysms)

I→C: direct Dx / DDx

I→C: patient subtyping



Prognosis

I→C: clinical score change, survival

I→C: high-risk/low-risk stratification (care / trial enrichment)



Treatment planning

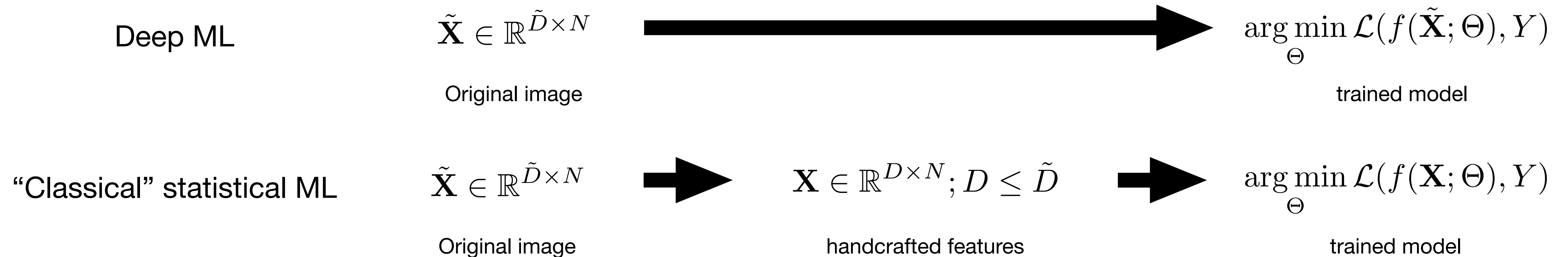
I→C: drug repurposing, responder/non-responder

How do we perform these analyses?

Imaging data are quite high-dimensional (in terms of voxels) compared to clinical data

Brain structural imaging - 4.6M voxels per image

Brain functional imaging - 82K voxels per time point (image), 37M per session



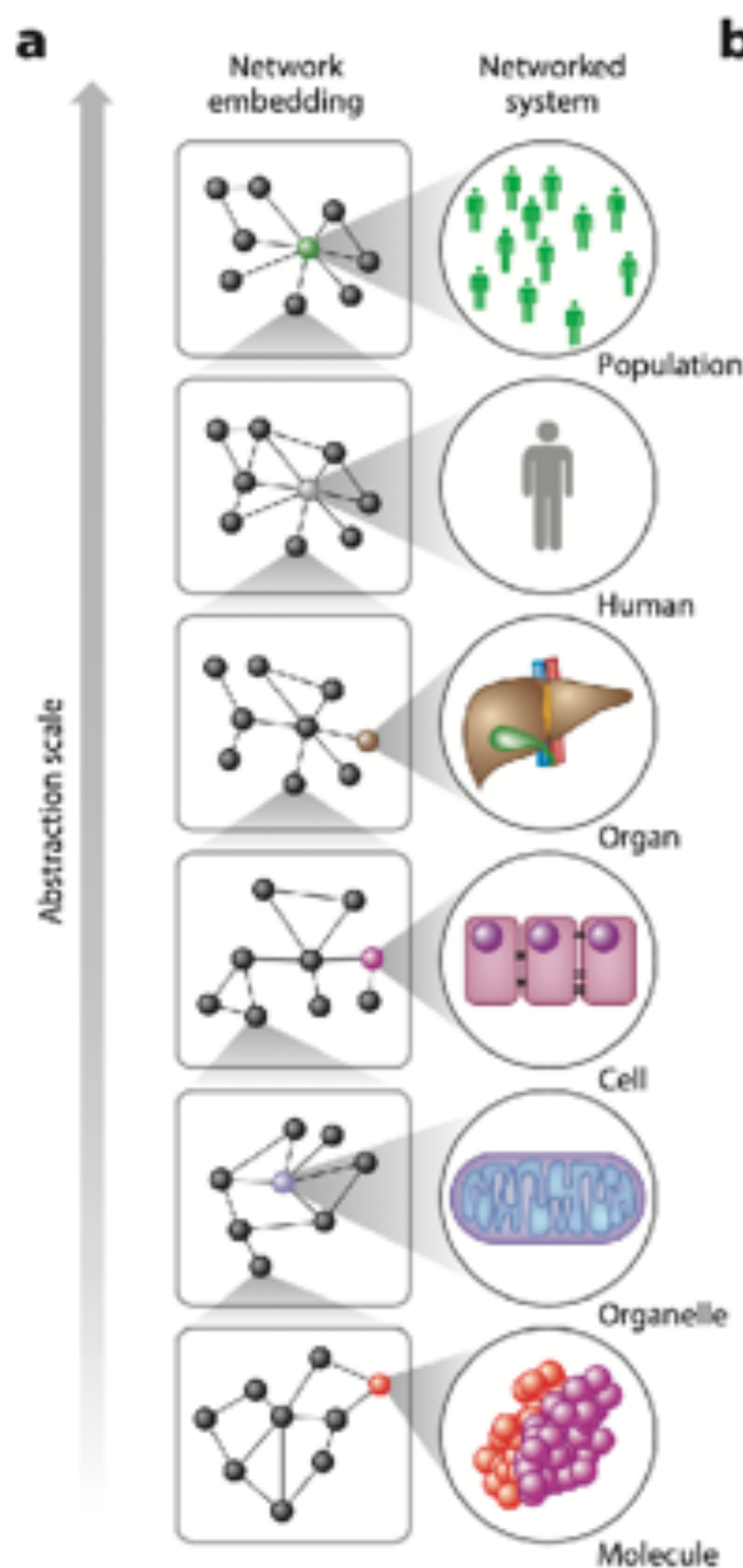
Use prior anatomical knowledge, signal processing, assumptions,
and analysis goals to define a lower-dimensional representation

Graphs in biology and biomedical imaging

Annual Review of Biomedical Data Science

Network Analysis as a Grand Unifier in Biomedical Data Science

Patrick McGillivray,¹ Declan Clarke,¹
William Meyerson,² Jing Zhang,^{1,2} Donghoon Lee,²
Mengting Gu,^{2,3} Sushant Kumar,¹ Holly Zhou,¹
and Mark Gerstein^{1,2,3}



(brain) graphs: a meso-scale representation for (brain) imaging analysis.

node = brain region
edge = “connection”
(structural or functional)



GeoMedia Workshop 2022

Geometric Deep Learning in Medical Image Analysis

Brain graphs and interpretability

Maladaptation

a Diaschisis

Dysfunction in remote regions



- Deafferentation
- Aberrant synchronization

b Transneuronal degeneration

Degeneration of remote regions



- Excitotoxicity
- Axonal transport
- Prion-like spread

c Dedifferentiation

Desegregated, non-specialized activity



- Altered neurodevelopment
- Impaired neuromodulation
- Deficient plasticity

Adaptation

d Compensation

Increased function in unaffected areas



- Plasticity
- Cognitive flexibility

e Neural reserve

Intact tissue sufficient to support function



- Limited pathology
- High reserve

f Degeneracy

Other systems assume function

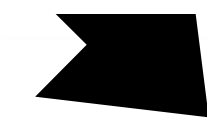
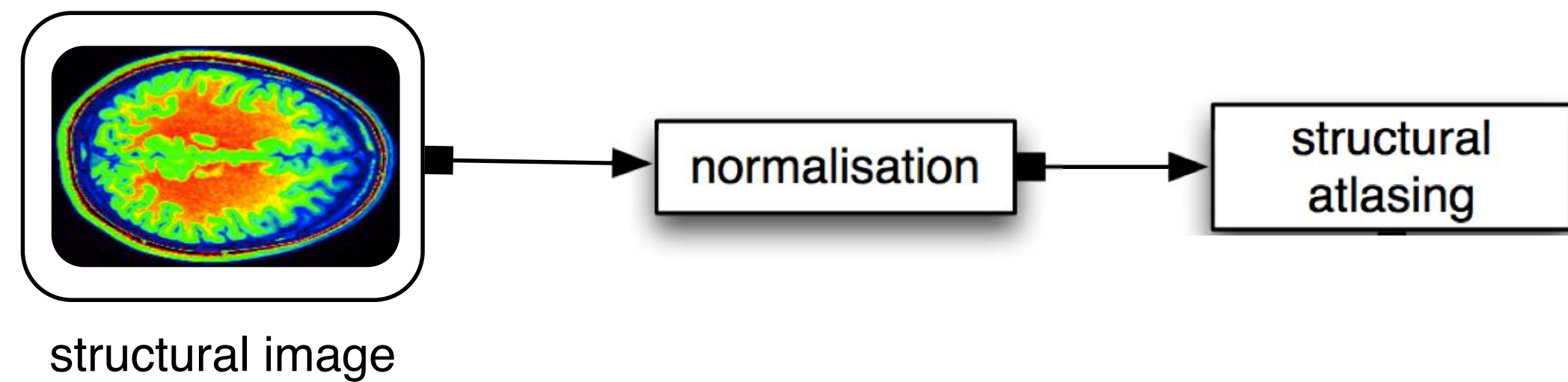


- Neurodevelopment
- Experience-dependent plasticity

■ Normal ■ Lesioned ■ Reduced activity ■ Increased activity

2. Graph estimation

From spatiotemporal brain imaging to graphs



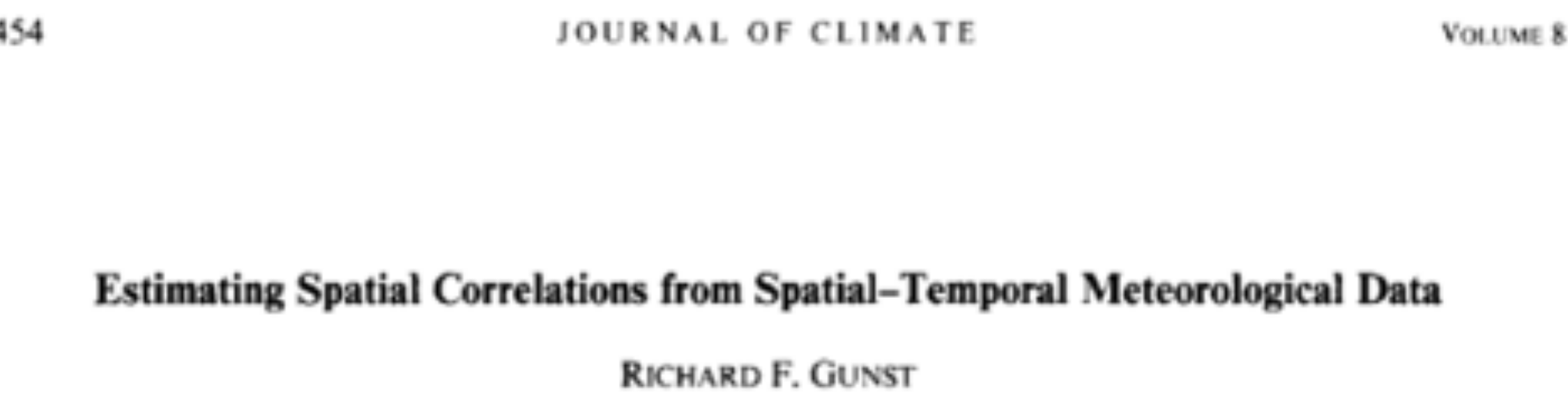
valid adjacency
matrix $\mathbf{A}$ (- diagonal)
for a weighted,
complete,
undirected graph

Inter-regional correlations

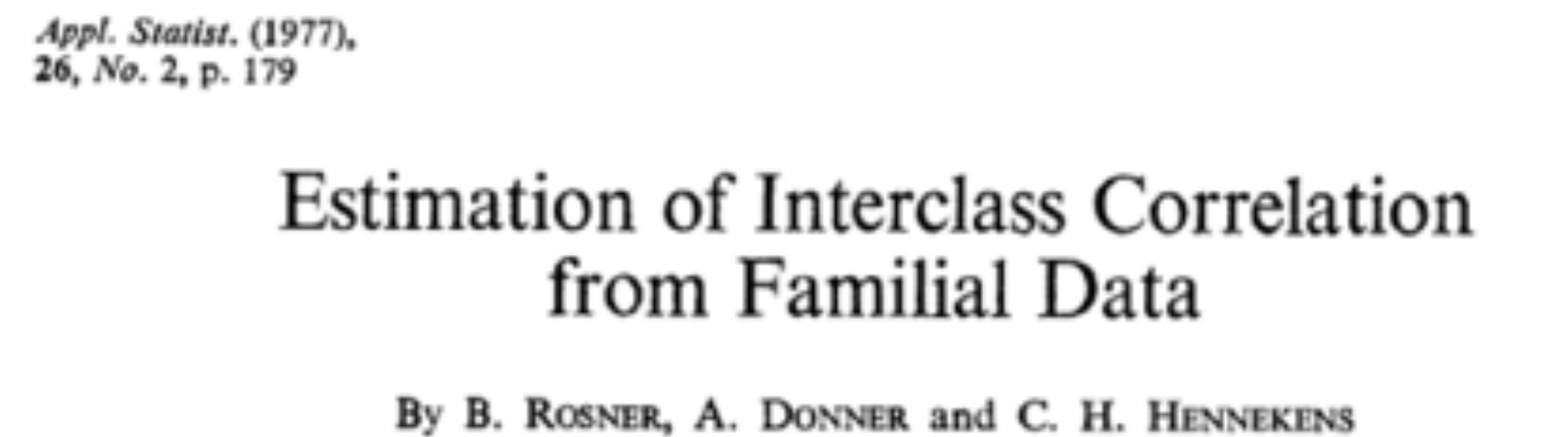
A problem with applications in many fields



[Gosset/Student, Biometrika, 1914]



[Gunst, J. Climate, 1995]



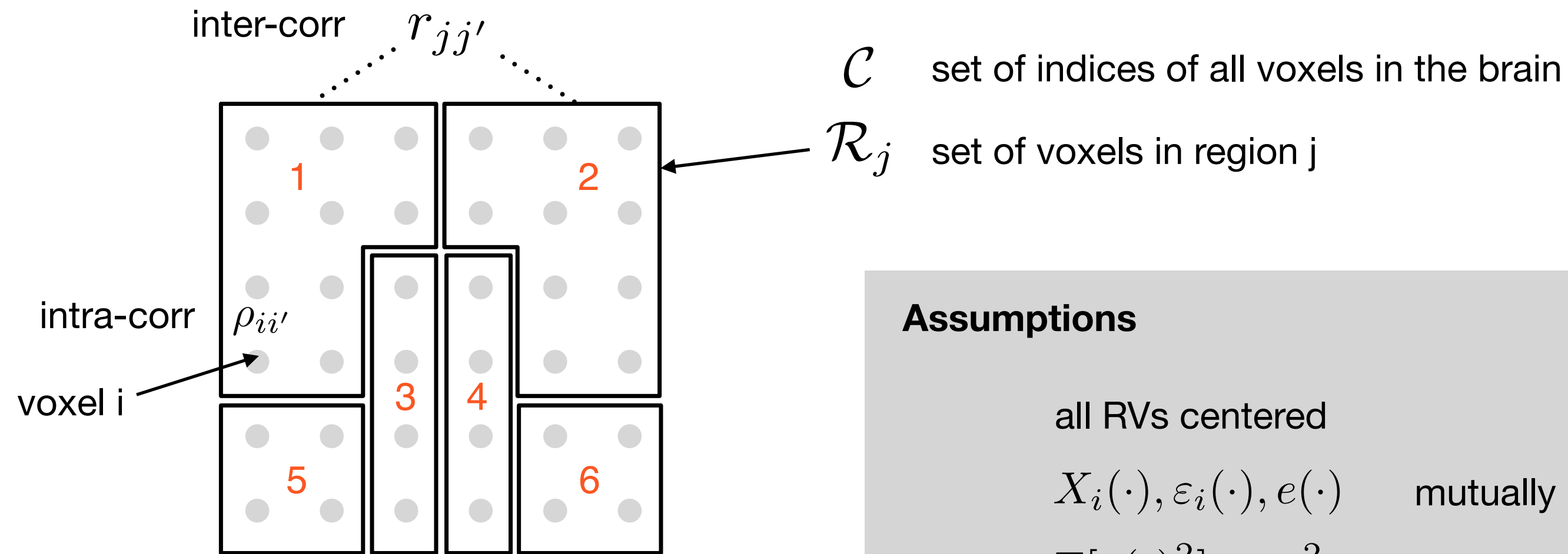
[Rosner et al, J. Royal Stat Soc. C (App. Statist.), 1977]



[Liebhold & Sharov, Proc. Int. Congress on Entomology 1996]

Inter-regional correlations

Notation, model, and assumptions



Signal model

$$Y_i(t) = X_i(t) + \varepsilon_i(t) + e(t)$$

Observed voxel value at time t (after DWT) Neural signal local noise global noise

Assumptions

all RVs centered

$X_i(\cdot), \varepsilon_i(\cdot), e(\cdot)$ mutually $\perp, \perp$ in time

$E[e(t)^2] = \sigma_e^2$ global noise homoskedastic

$\rho_{ii'} \approx 1$
 $(X_i(t), i \in \mathcal{R}_j), (\varepsilon_i(t), i \in \mathcal{C})$

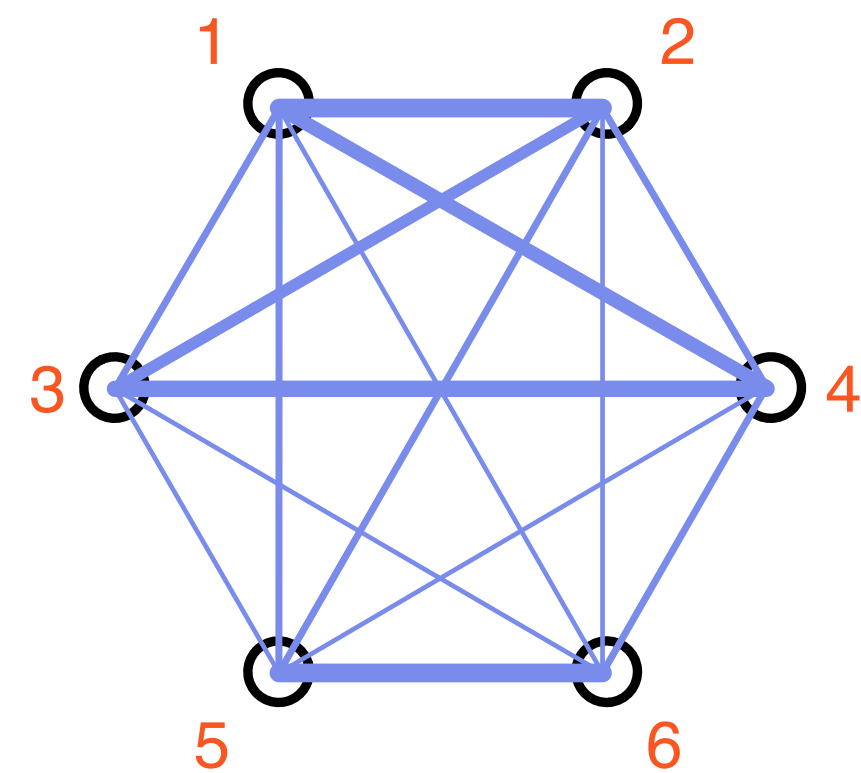
$\forall (i, i', j) \rho_{ii'} \in \mathcal{R}_j$

$\forall (i, i', j) \eta_{ii'} \in \mathcal{R}_j$

for small distances

stationary random fields

stationary and isotropic with respect to distance



Covariance model under assumptions

inter-regional correlation = parameter of interest

global noise variance

$$\text{cov}(Y_i(t), Y_{i'}(t)) = \begin{cases} \sigma_j \sigma_{j'} r_{jj'} + \sigma_e^2 & \text{if } j \neq j' \\ \sigma_j^2 \rho_{ii'} + \sigma_\varepsilon^2 \eta_{ii'} + \sigma_e^2 & \text{if } j = j' \end{cases}$$

intra-region correlation

local noise correlation

(OLD PREPRINT) [Achard, Coeurjolly, Lafaye de Micheaux and Richiardi <https://arxiv.org/abs/2011.08269>, 2020]

Inter-regional correlations

Estimators (selected from 9)

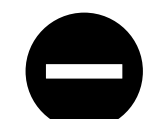
Desirable properties: 1) handle regions with different number of voxels , 2) handle small intra-correlations, 3) robust to local noise, (4) robust to global noise)

“correlation of averages”

$$\hat{r}_{jj'}^{\text{CA}} = \frac{\widehat{\text{COV}}(\bar{\mathbf{Y}}_{\mathcal{R}_j}, \bar{\mathbf{Y}}_{\mathcal{R}_{j'}})}{\hat{\sigma}(\bar{\mathbf{Y}}_{\mathcal{R}_j})\hat{\sigma}(\bar{\mathbf{Y}}_{\mathcal{R}_{j'}})}.$$



local noise: smoothed



size effect: highly dependent on intra-correlations: estimate for

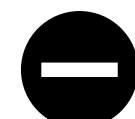
$$r_{jj'} / \sqrt{\bar{\rho}_{\mathcal{R}_j} \bar{\rho}_{\mathcal{R}_{j'}}}$$

can degenerate if regions are not positively intra-correlated enough

fMRI: e.g. [Achard et al, J. Neurosci, 2006]

“average of correlations”

$$\hat{r}_{jj'}^{\text{AC}} = \frac{1}{N_j N_{j'}} \sum_{i \in \mathcal{R}_j, i' \in \mathcal{R}_{j'}} \widehat{\text{COR}}(\mathbf{Y}_i, \mathbf{Y}_{i'}).$$



local noise: not robust



size effect: corrected

“local correlation of averages”

$$\hat{r}_{jj'}^{\ell\text{CA}} = \frac{1}{B} \sum_{b=1}^B \widehat{\text{COR}}(\bar{\mathbf{Y}}_{\mathcal{V}_j^{(b)}}, \bar{\mathbf{Y}}_{\mathcal{V}_{j'}^{(b)}}).$$



local noise: smoothed



size effect: corrected

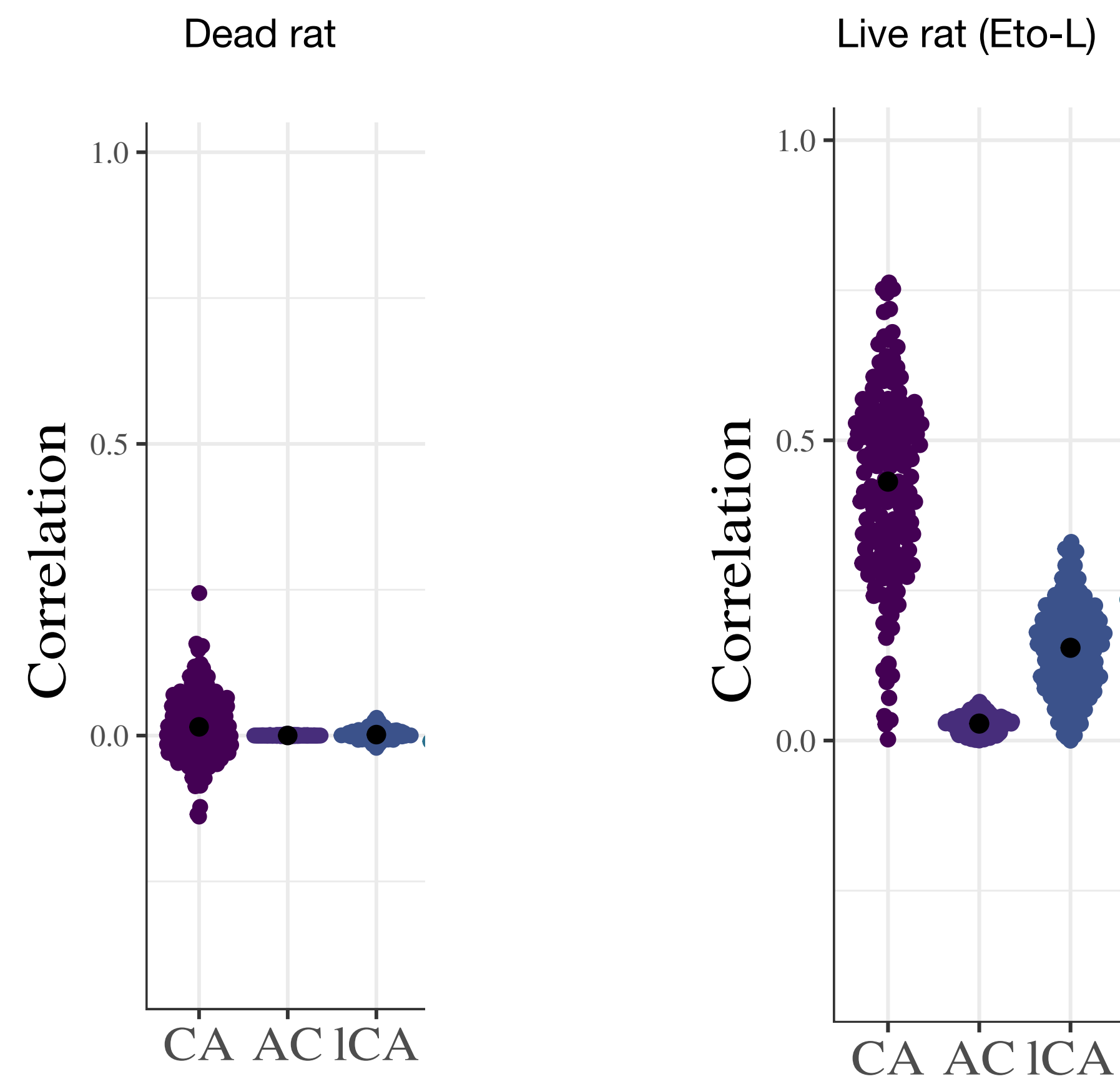
[Achard et al, IEEE SSP, 2011]

[Achard, Coeurjolly, Lafaye de Micheaux, Lbath and Richiardi, in prep.]

Inter-regional correlations

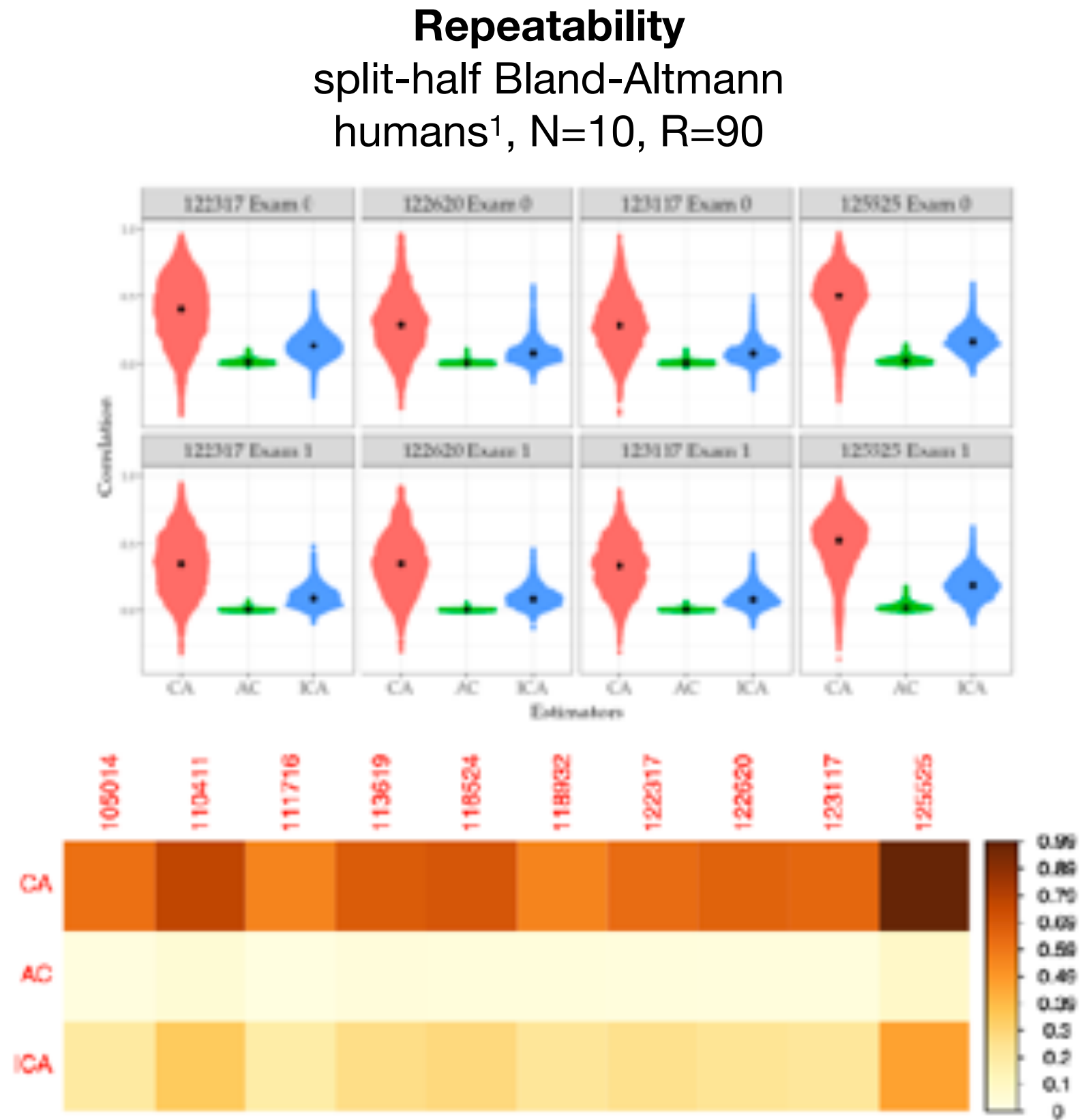
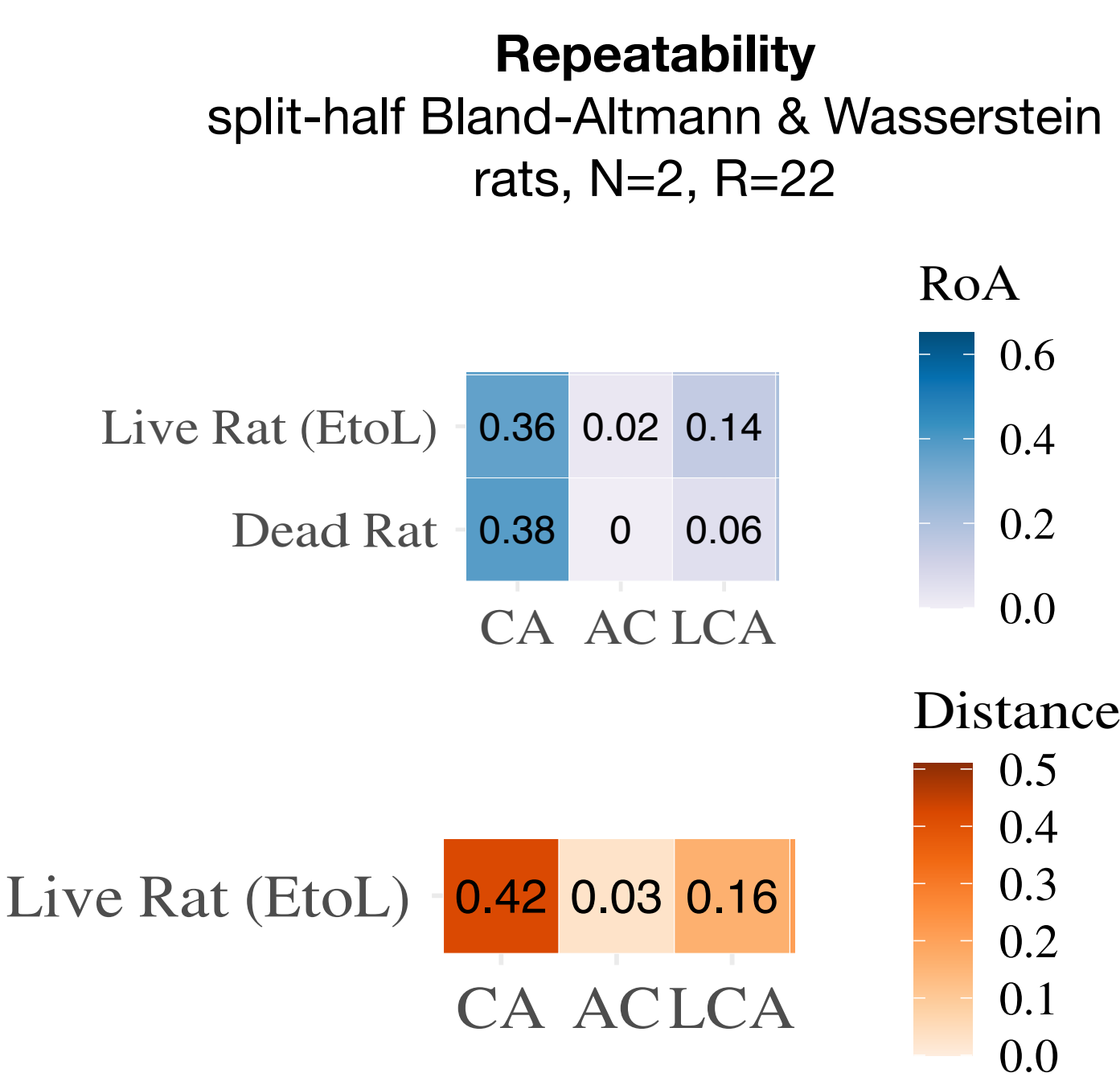
Empirical results - face validity

live vs dead rats
rats, N=2, R=22



Inter-regional correlations

Empirical results - repeatability & discriminative power



Discriminative power
fingerprinting² & direct embedding distance
humans, N = 10, R=90

estimator	CA	AC	LCA
intra-subject mean (sd)	0.36 (0.15)	0.27 (0.13)	0.35 (0.14)
inter-subject mean (sd)	0.60 (0.18)	0.46 (0.17)	0.57 (0.17)
W	-3.95	-3.36	-3.58
p	3.9x10 ⁻⁵	3.9x10 ⁻⁴	1.7x10 ⁻⁴
identification rate	80%	50%	60%

Conclusion: LCA has face validity, seems to offer increased repeatability, possibly at the expense of discriminative power

¹Human data <https://humanconnectomeproject.org> [Achard, Coeurjolly, Lafaye de Micheaux, Lbath and Richiardi, in prep.] ²[Finn et al., Nature Neuroscience, 2015]

Inter-regional correlations

Limitations

Filtering: bandpass filtering

Aggregation: decomposition approaches (ICA, EMD, EEMD...)

Non-linear/causal estimators: Mutual Information, Granger Causality, ...

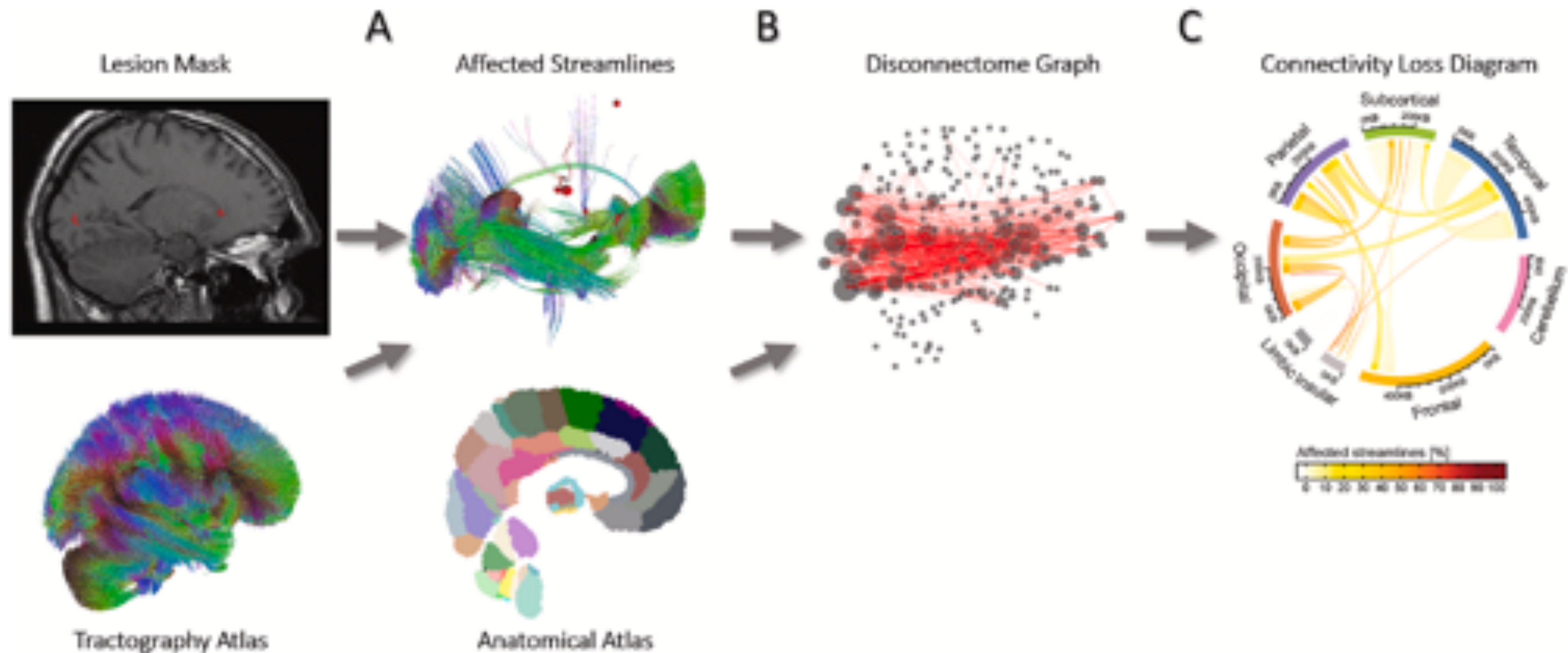
Full structure learning: partial correlation, inverse covariance, PC*...

Regularisation: Ledoit-Wolfe, gLasso...

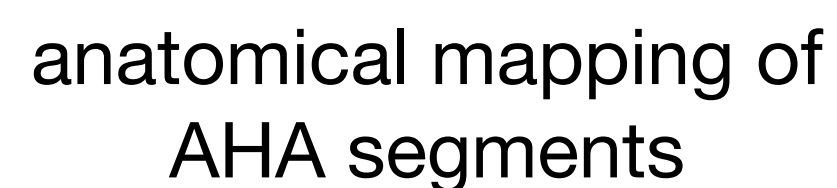
Noise: multiplicative, convolutional...

Brain disconnectomics

Atlas-based estimation of white matter tract damage in MS



Compact representation of cardiac structure and function

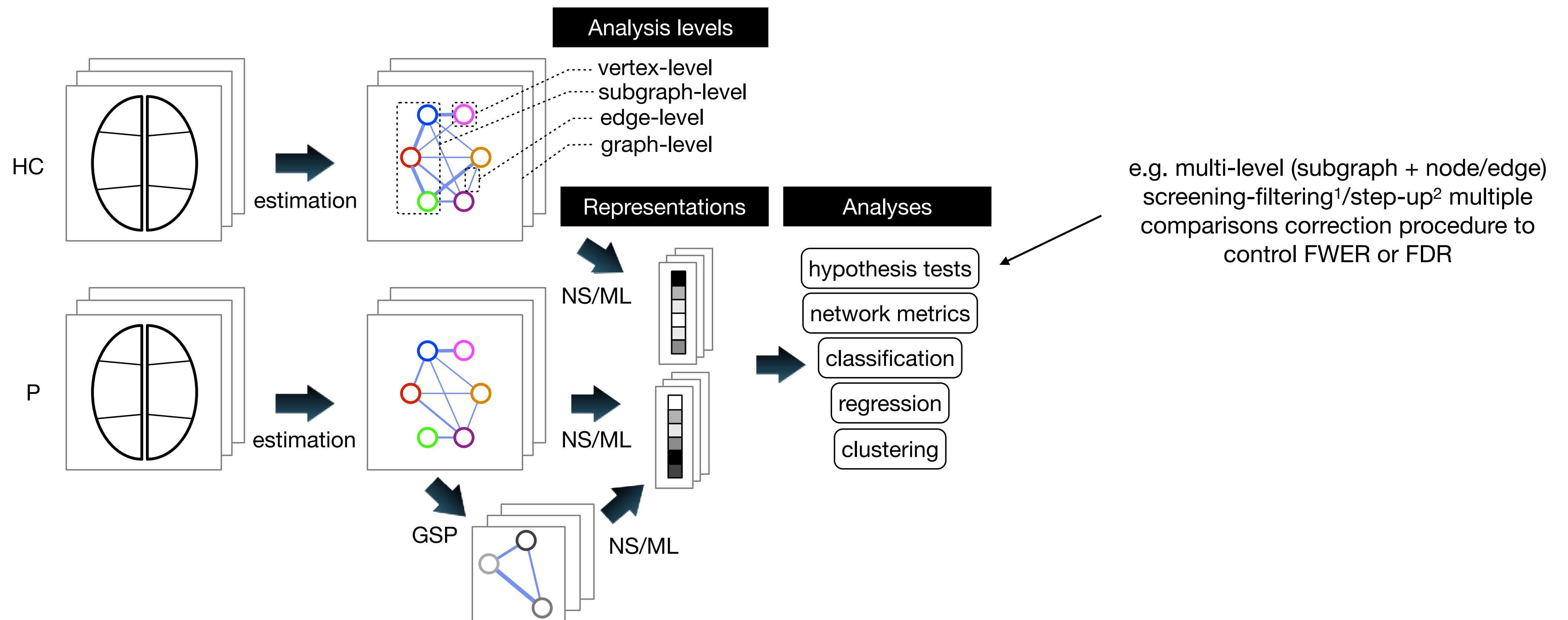


building labelled graphs with edge labels and vertex labels

example dilated cardiomyopathy
patient graph, end-diastole (top) and
end-systole (bottom)

3. Graph analysis

Analysis levels, representations, and approaches

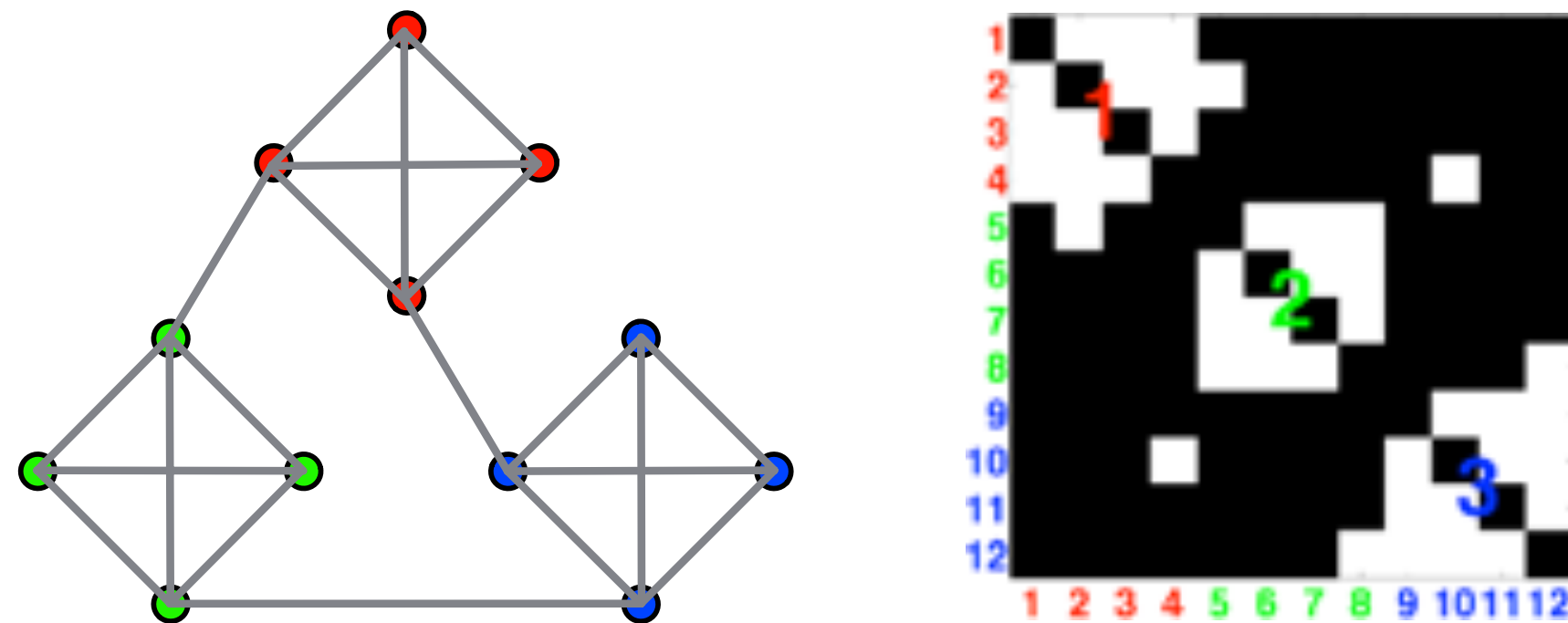


Network science approaches

Focus on subgraphs or topological properties

Principle

Brain graphs have identifiable subgraphs (“modules”, “communities”) in several modalities



The partition into communities can be used to compare brain graphs between subjects at various scales

Whole-brain: graphwise community structure

“Subnetwork of regions”: individual communities

Single region: community membership (not shown)

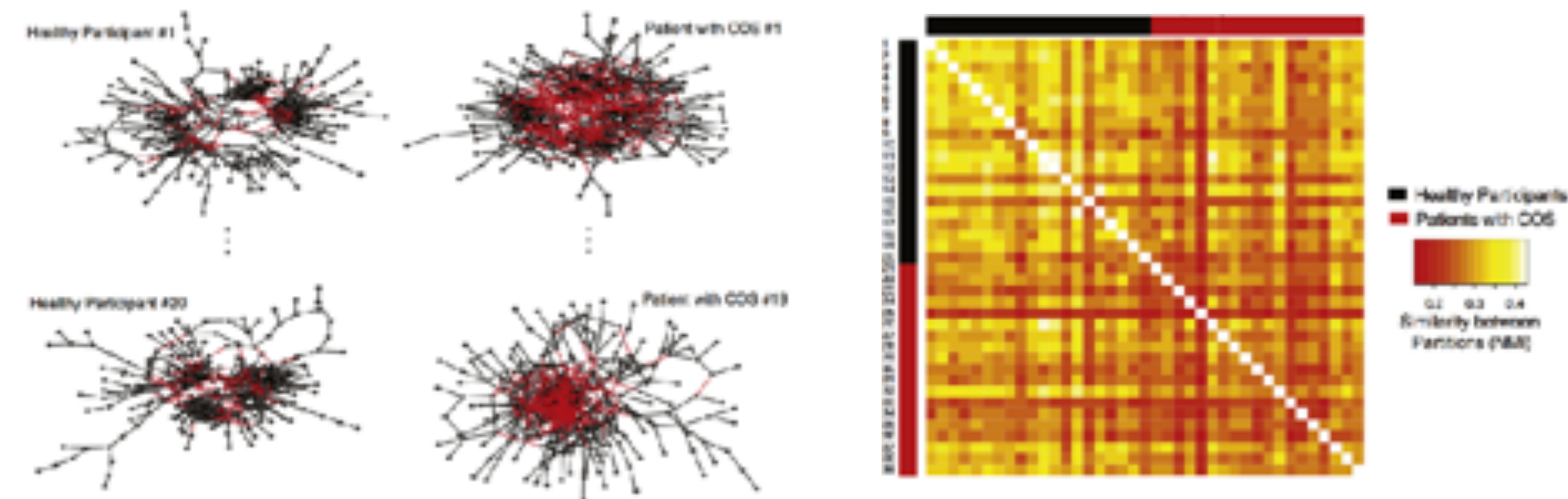
Application

Goal: discriminate patients with schizophrenia

Data: fMRI, 23 HC, 23 SZ, TR=2.3s, rest, 2x3 min (144 points)

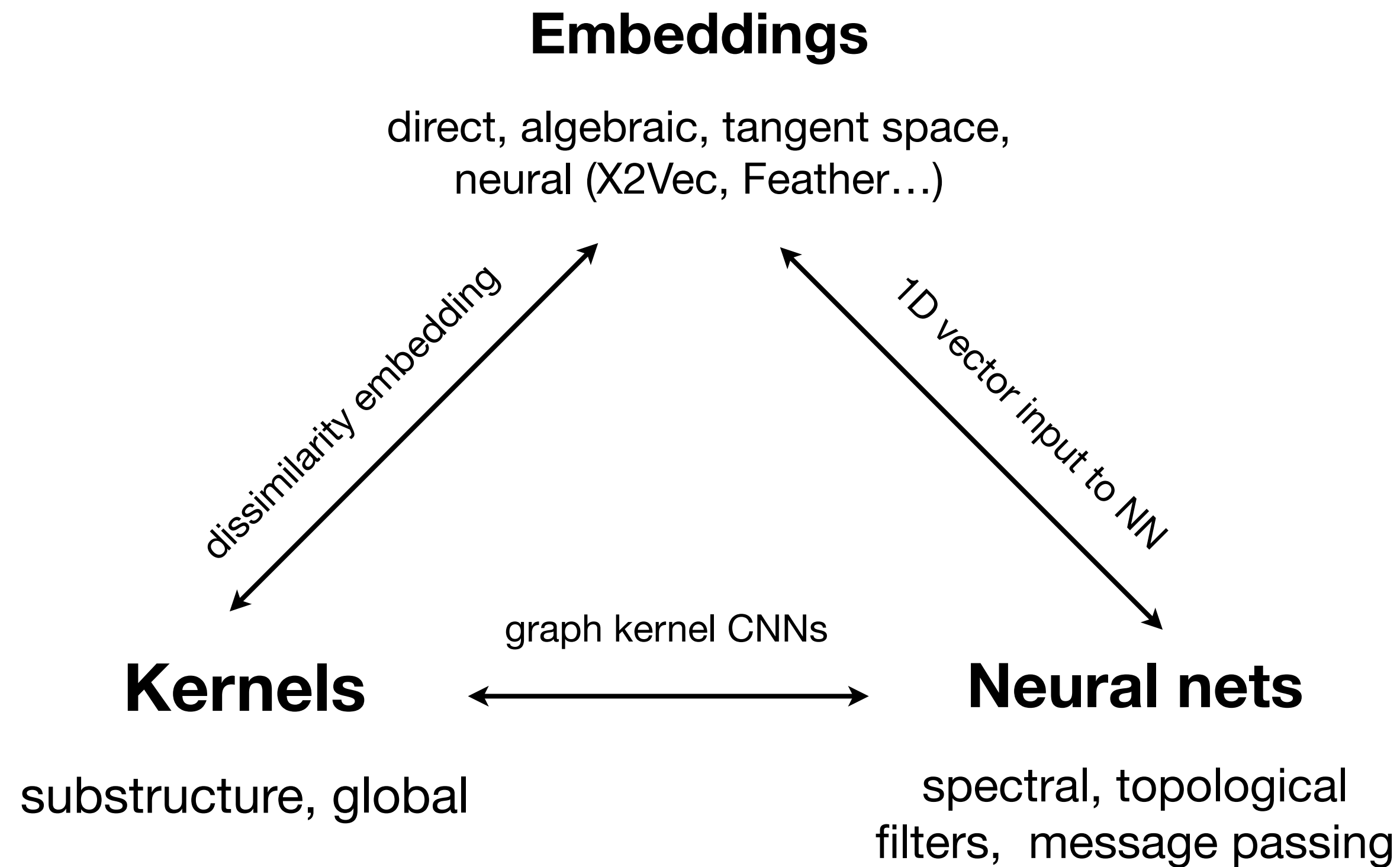
Vertices: Subparcellated Harvard-Oxford, 278 regions

Edge labels: thresholded and binarised absolute wavelet correlation, 0.05-0.1Hz



[Alexander-Bloch et al., NeuroImage, 2012]

Machine learning approaches



Graph embeddings

Graph embedding maps graphs to points in $\mathbb{R}^D$

With G a set of graphs, a graph embedding $\varphi : G \rightarrow \mathbb{R}^D$
maps graphs to D-dimensional vectors:

$$\varphi(g) = (x_1 \dots x_D)^T$$

For brain graphs, we are generally interested in preserving edge label information

Vertex labels can be dropped because of the correspondence between atlas regions

Once we have vectors we can use any ML algorithm we want

Direct embedding and behaviour/phenotype prediction

Principle

Use the upper-triangular part of $\mathbf{A}^{1,2,3}$

$$\begin{pmatrix} (1, 1) & \dots & (1, |V_i|) \\ & \ddots & \\ & & (|V_i|, |V_i|) \end{pmatrix} \longrightarrow \begin{pmatrix} (1, 2) \\ \vdots \\ (|V_i| - 1, |V_i|) \end{pmatrix}$$

$$\mathbf{A}_i \in \mathbb{R}^{|V_i| \times |V_i|} \qquad \mathbf{a}_i \in \mathbb{R}^{\binom{|V_i|}{2} \times 1}$$

“Cursed” representation and loss of posdefness,
but generally a competitive baseline (at least with
~100 vertices, fMRI)

Links Mantel test statistic with Linear kernel SVM - same notion of similarity

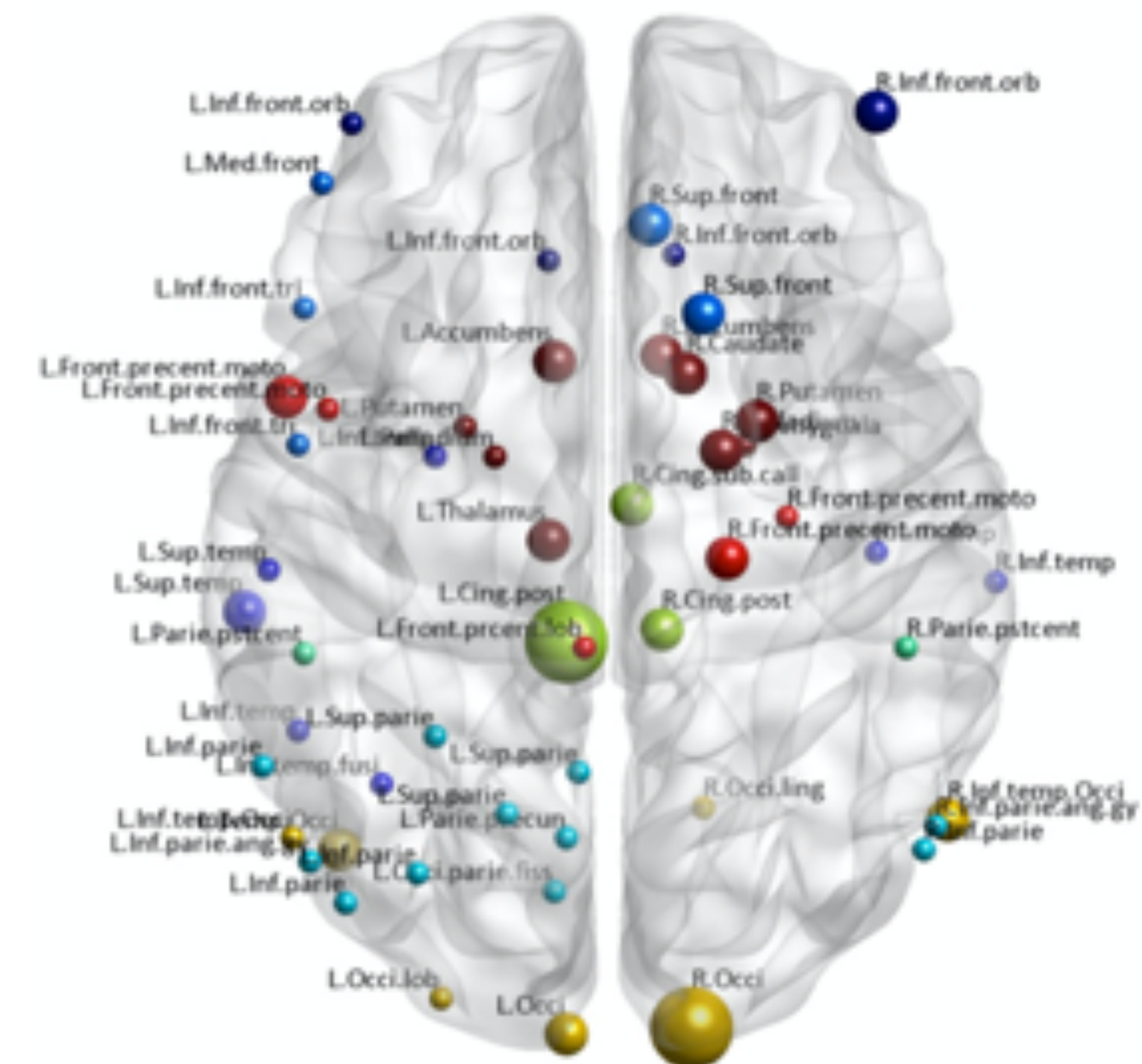
Application

Task: Dx, 30 depressive vs 30 matched HC

Data: task fMRI, 137 regions

Classifier: L1-SVM on direct embedding

Results: 85% acc



¹ [Wang et al., MICCAI, 2006]

2 [Craddock et al., MRM, 2009]

3 [Richiardi et al., ISBI 2010]

[Richiardi et al., ICPR 2010]

[Richiardi et al., NeuroImage, 2011+12]

[Rosa et al., Neuroimage, 2015]

Graph convolutional networks and phenotype prediction

Principle¹

Approximate spectral filtering on graphs²

$$H^{(l+1)} = \sigma(\tilde{D}^{-\frac{1}{2}} \tilde{A} \tilde{D}^{-\frac{1}{2}} H^{(l)} W^{(l)})$$

Degree matrix layer activations

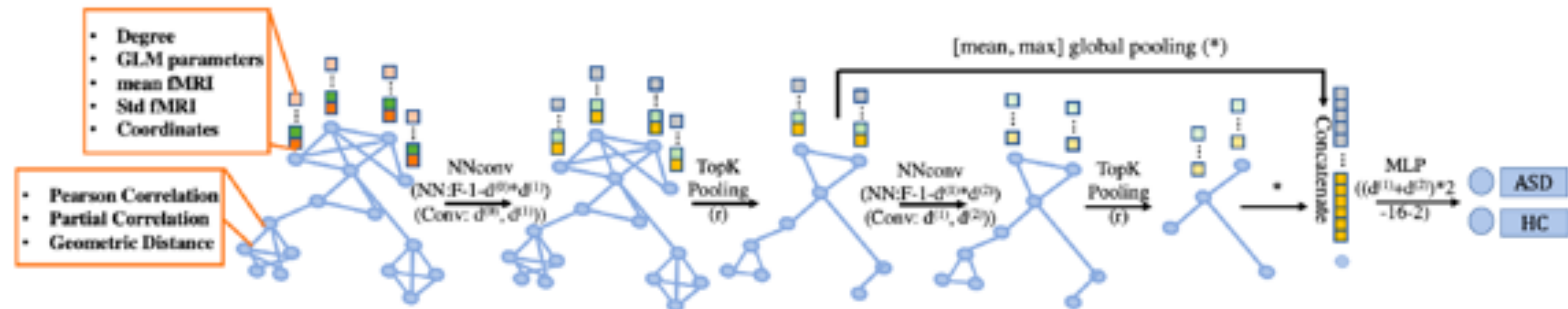
A+I layer weight matrix (trainable)

¹[Kipf and Welling, ICLR, 2017]

²[Cvetkovic et al., Spectra of Graphs, AP, 1980] [Luo et al., Pattern Recognition, 2003] [Deferrard et al., NeurIPS, 2016]

Application

Task: Dx, 75 ASD depressive vs 43 matched HC
Data: task fMRI, 148 regions
Classifier: GNN with edge and node attributes
Results: 76% acc

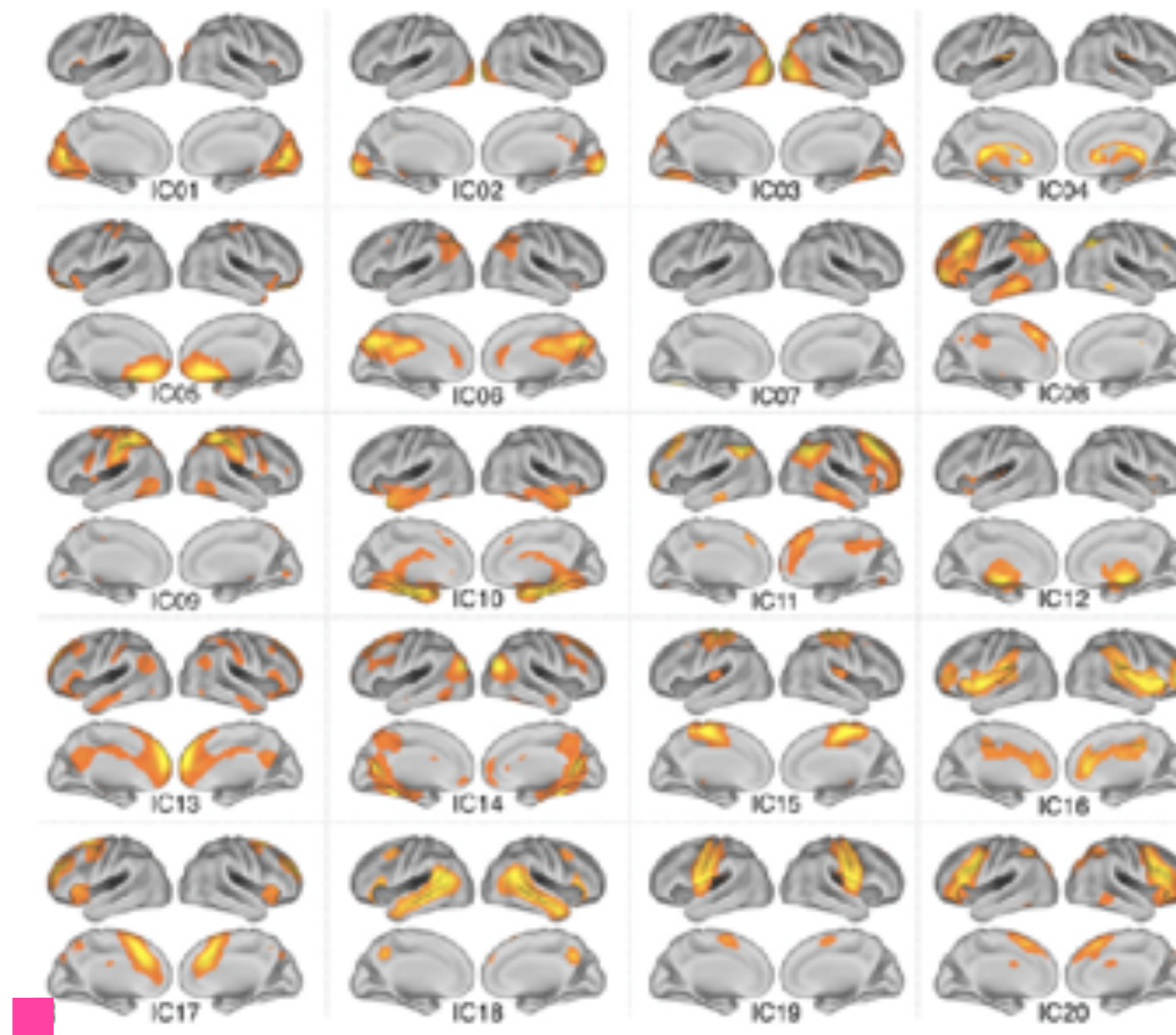


[Li et al., MICCAI, 2019]

4. Graph imaging genetics

Genetics of intrinsic brain activity

In humans and lower mammals, spatially consistent, synchronised, intrinsic activity forming “functional networks” is observed reproducibly across the lifespan



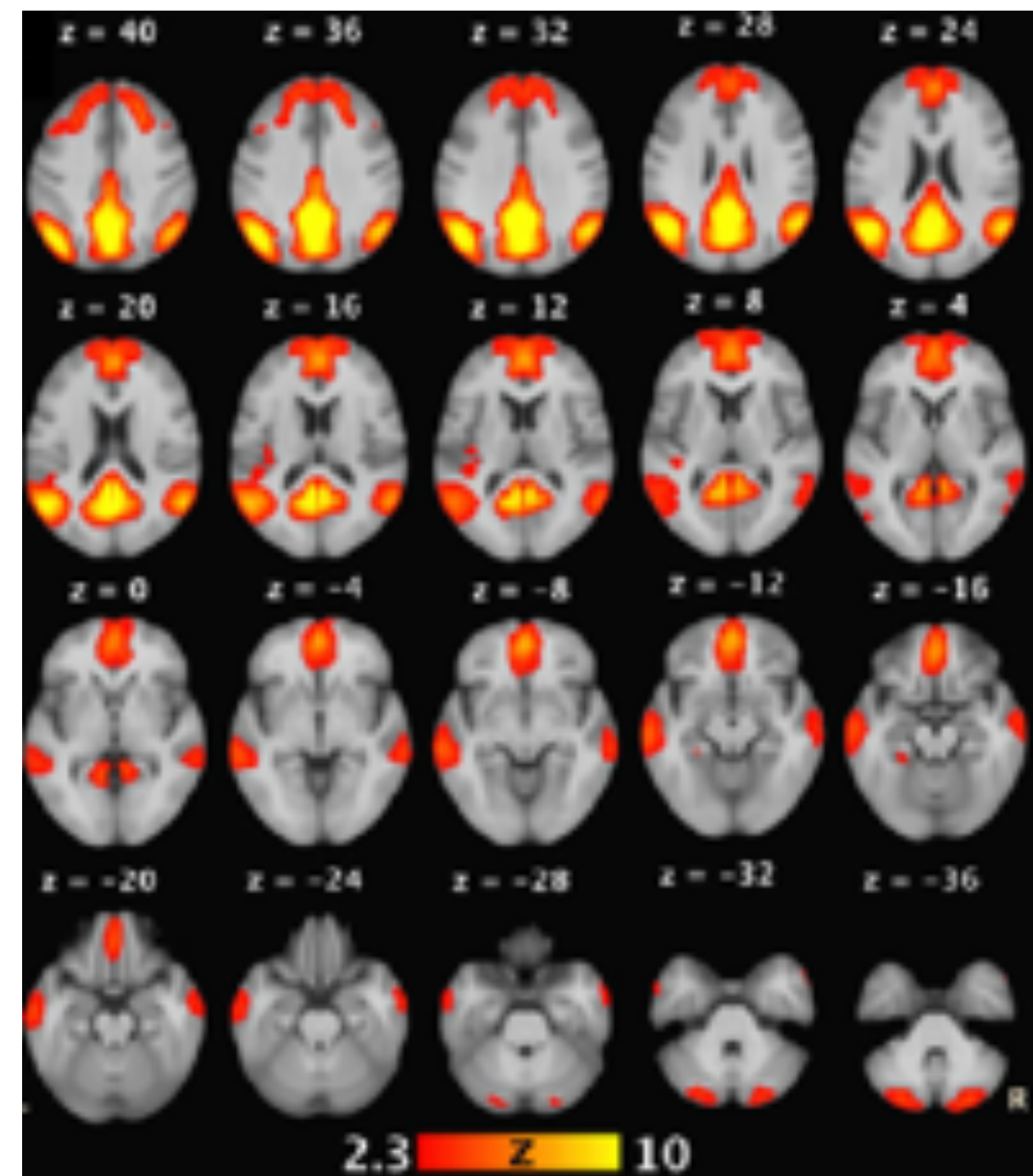
BOLD fMRI, ICA(K=20), N=1093, C=24

What are the genetic correlates of this consistency?

Functional networks are heritable

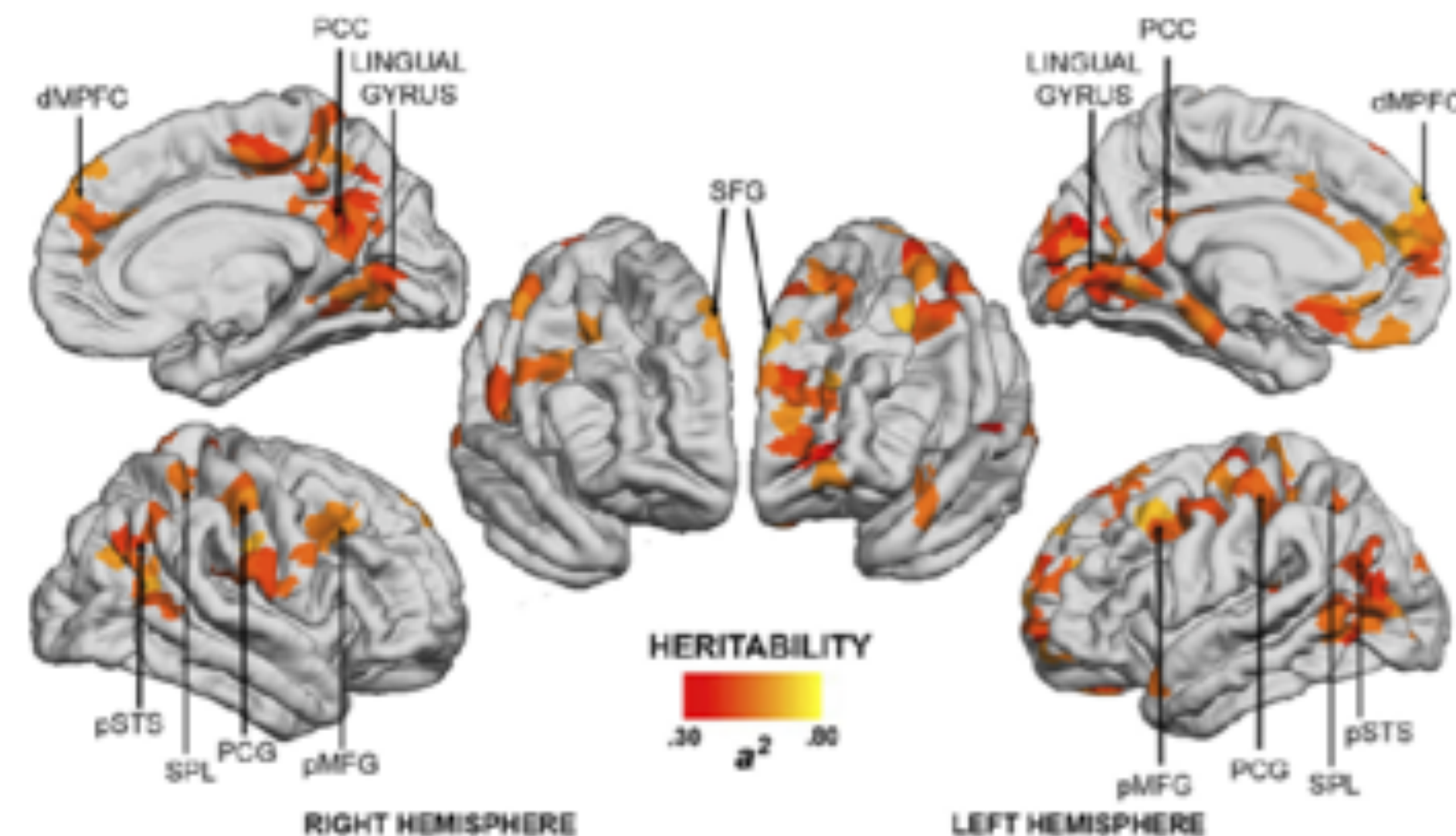
Like other neuroimaging phenotypes^{1,2}, some aspects of FNs are heritable

Connectivity within the DMN is heritable³ (0.4, $p=0.005$)



BOLD fMRI, ICA (K=17), N=333

Some topological metrics of FNs are heritable⁴ (0.6 for CE)



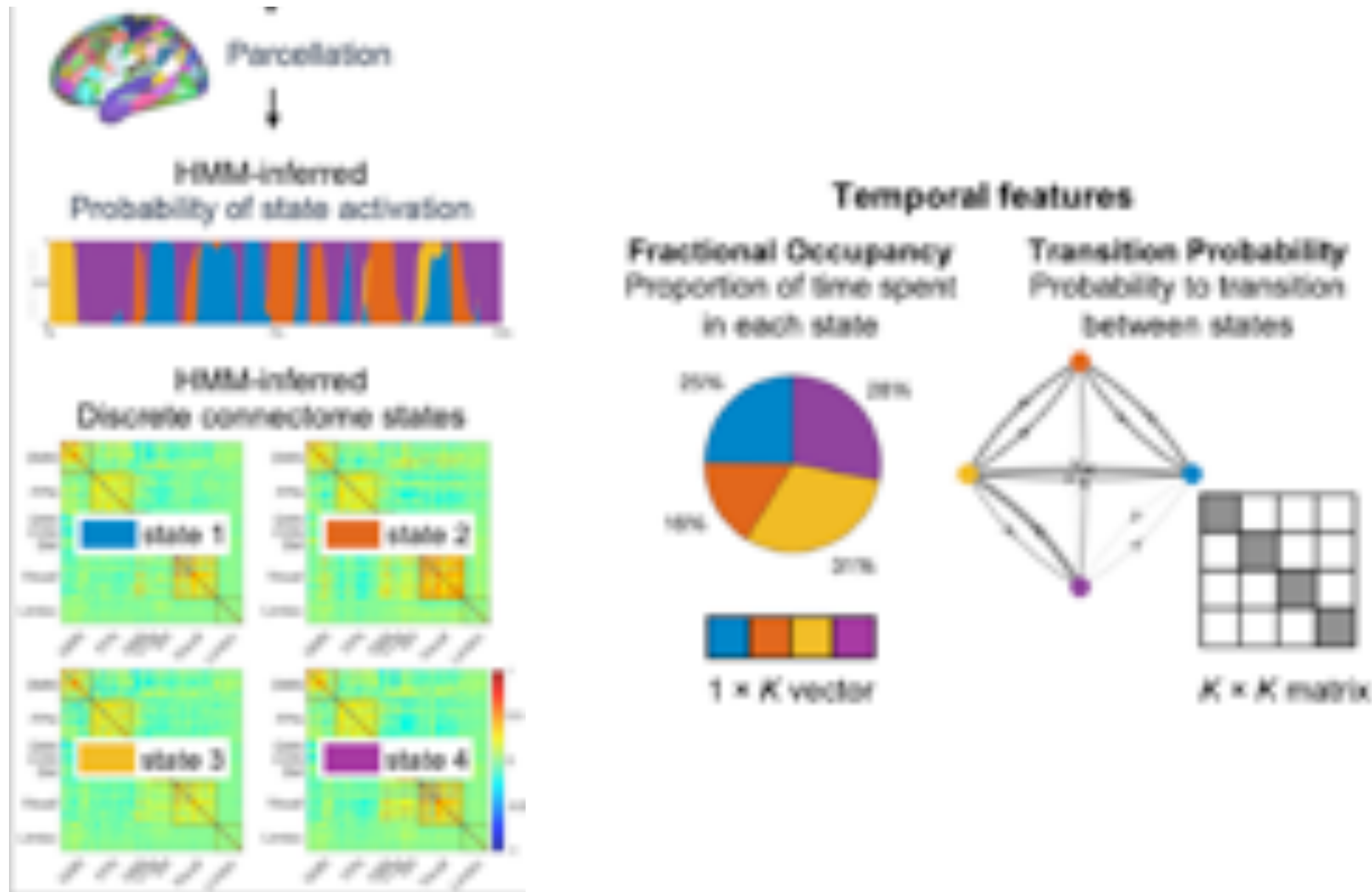
BOLD fMRI, R=1041, N=48

¹[den Braber et al., NeuroImage, 2013]

²[Chiang et al., J. Neurosci, 2009]

28 ³[Glahn et al., PNAS 2010]⁴[Fornito et al., J. Neurosci, 2011]

Dynamics of functional networks are also heritable



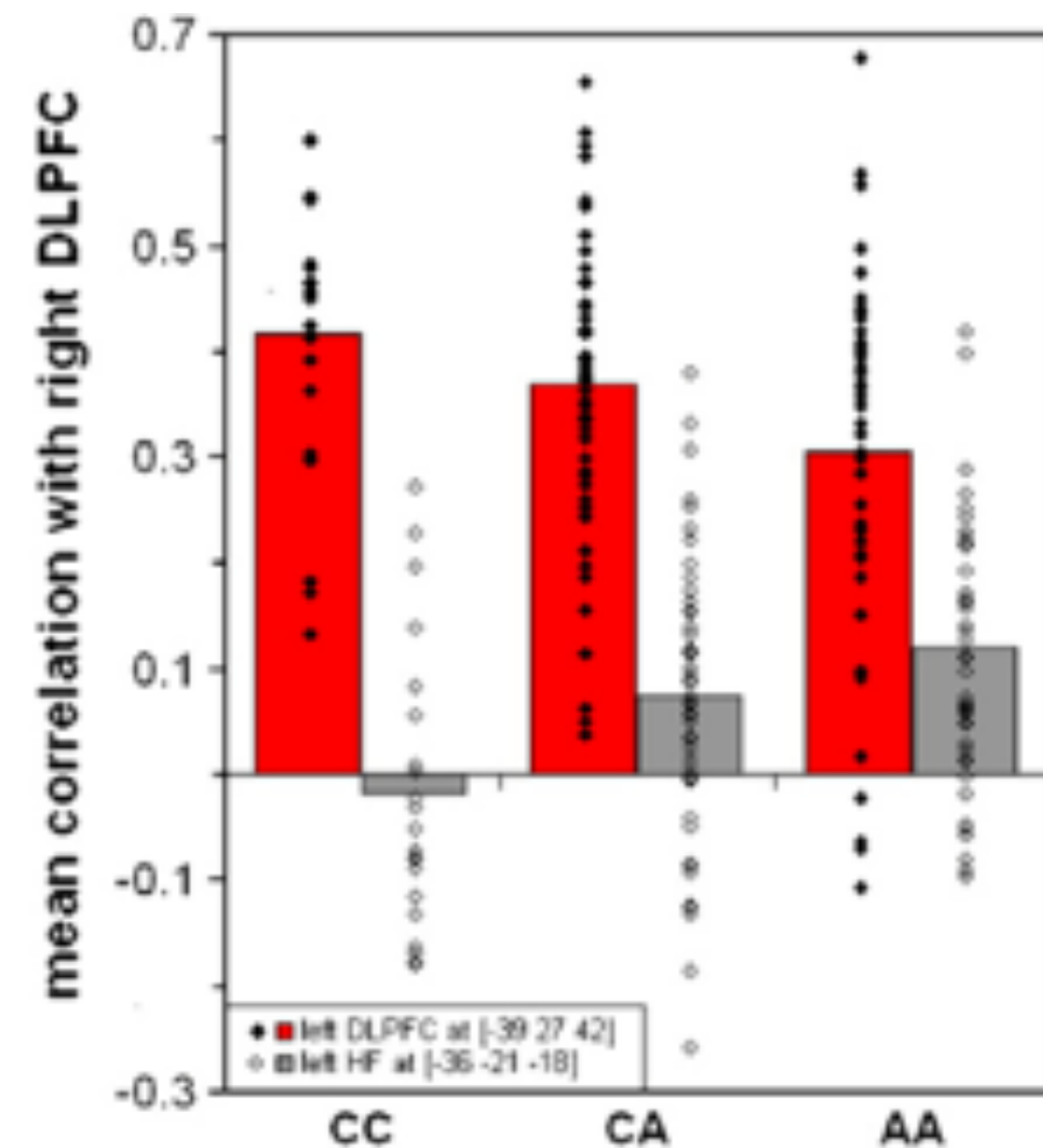
N=1003 (aged 22–37, 534 females):
120 monozygotic (MZ) twin pairs
65 sex-matched dizygotic (DZ) twin pairs
96 sex-matched non-twin (NT) sibling pairs
62 pairs of sex-matched unrelated individuals.

($h^2=0.39$, 95% CI= [.24,.54] for FO
 $h^2=0.43$, 95% CI=[.29,.57] for TP)

SNPs modulate functional networks

Genetic risk factors for many diseases affect FNs¹

ZNF804 / rs1344706 (SZ risk)²

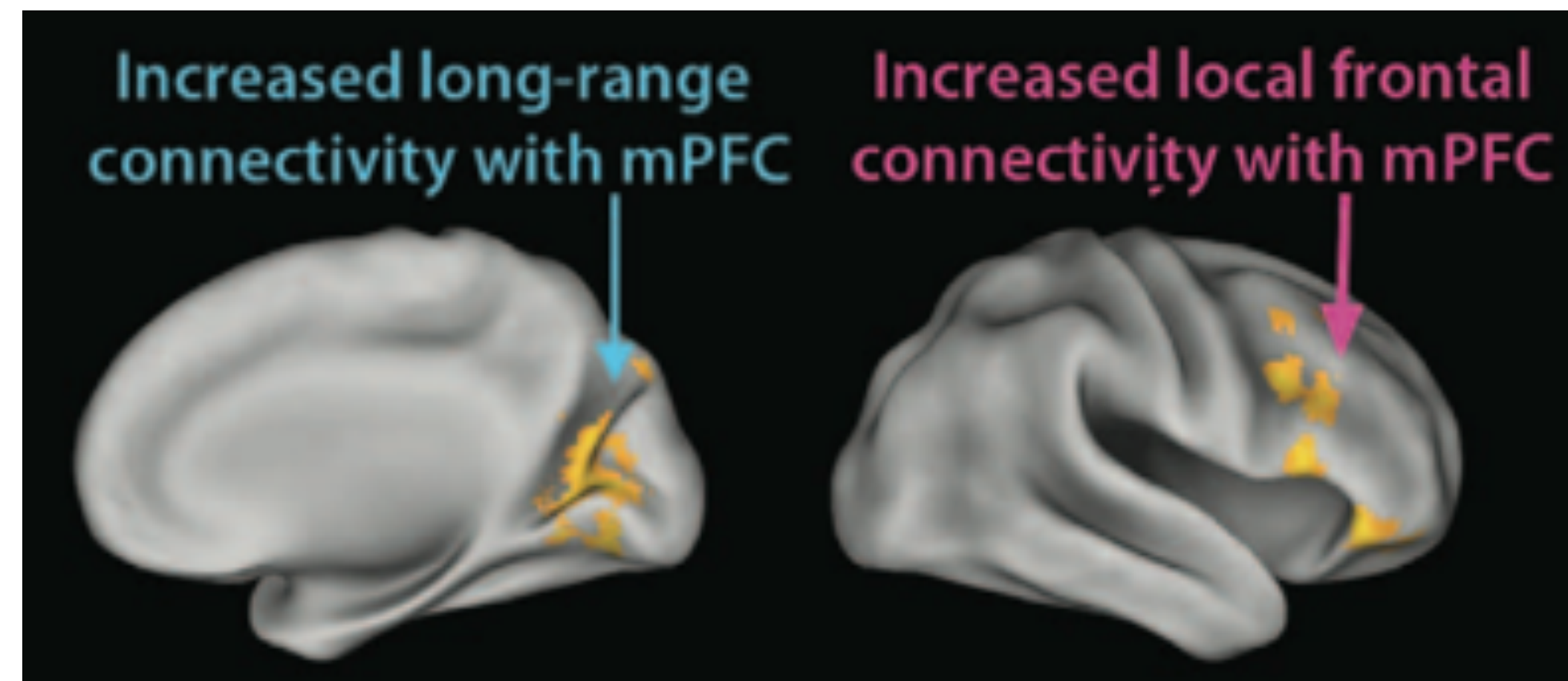


BOLD fMRI, *seed corr*, N=115 HC

CNTNAP2 / rs2710102 (ASD risk)³

nonrisk>risk

risk>nonrisk



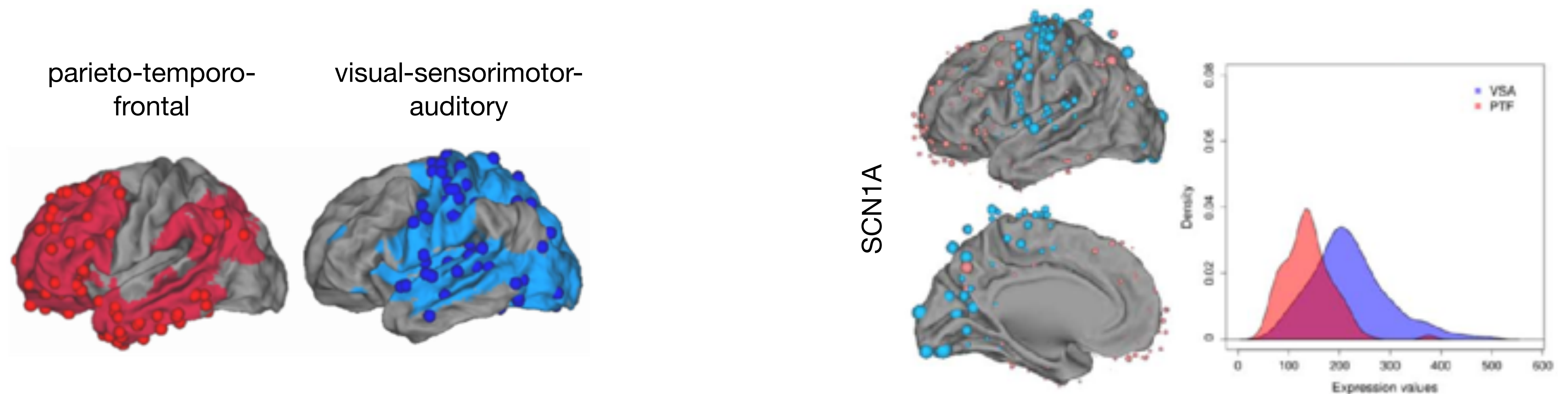
BOLD fMRI, *seed corr*, N=71 (16+39 HC, 16 ASD)

¹[Tost et al., Neuroimage, 2012] ²[Esslinger et al., Science, 2009]

³[Scott-Van Zeeland et al., Science Transl. Med., 2010]

Gene expression relates to functional networks

Different (cortical) FNs¹ have different gene expression²



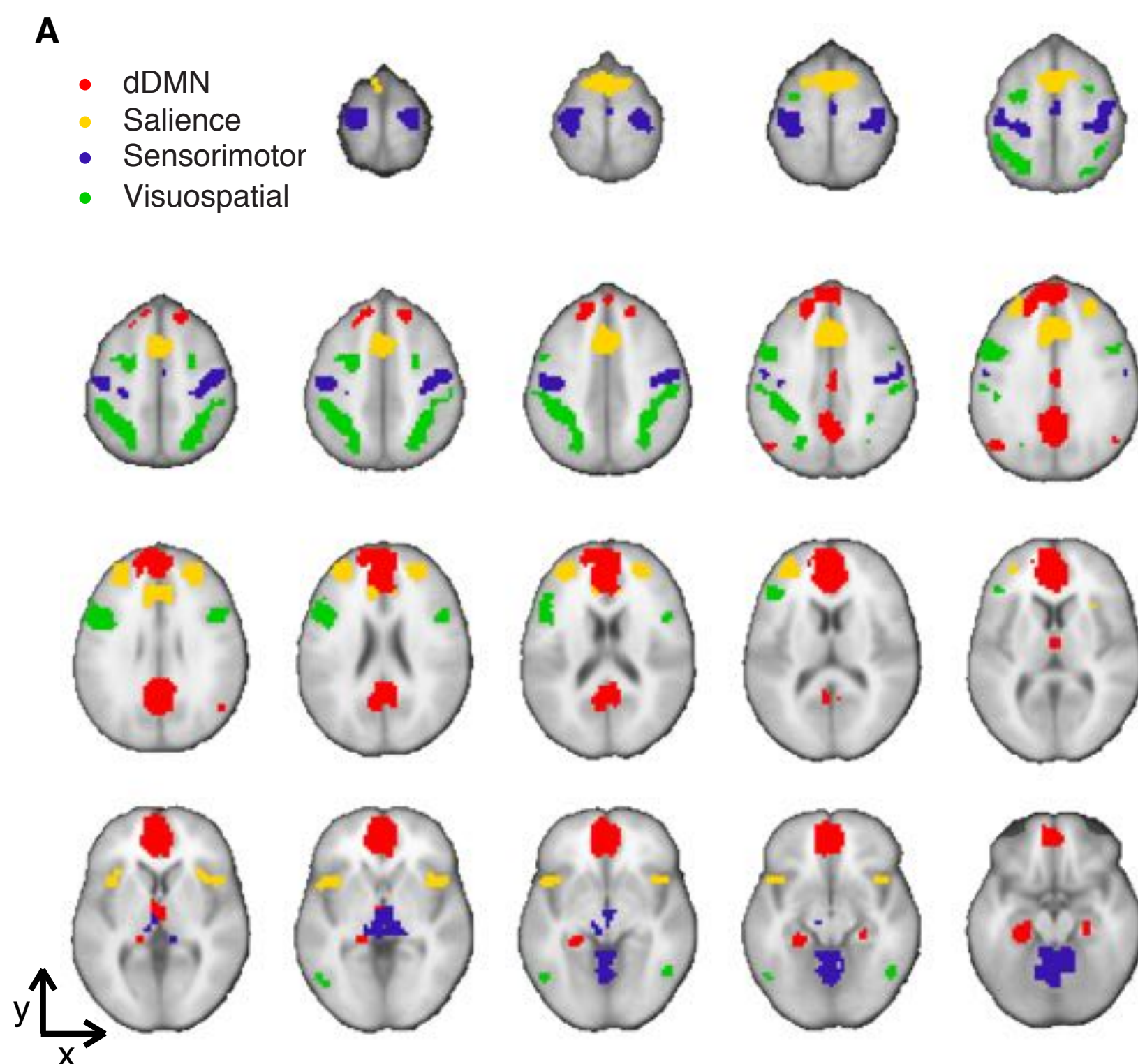
N=1 (394 samples), G=938

¹[Mesmoudi et al., PLoS one, 2013] (dual rings)

²[Cioli et al., PLoS one, 2014]

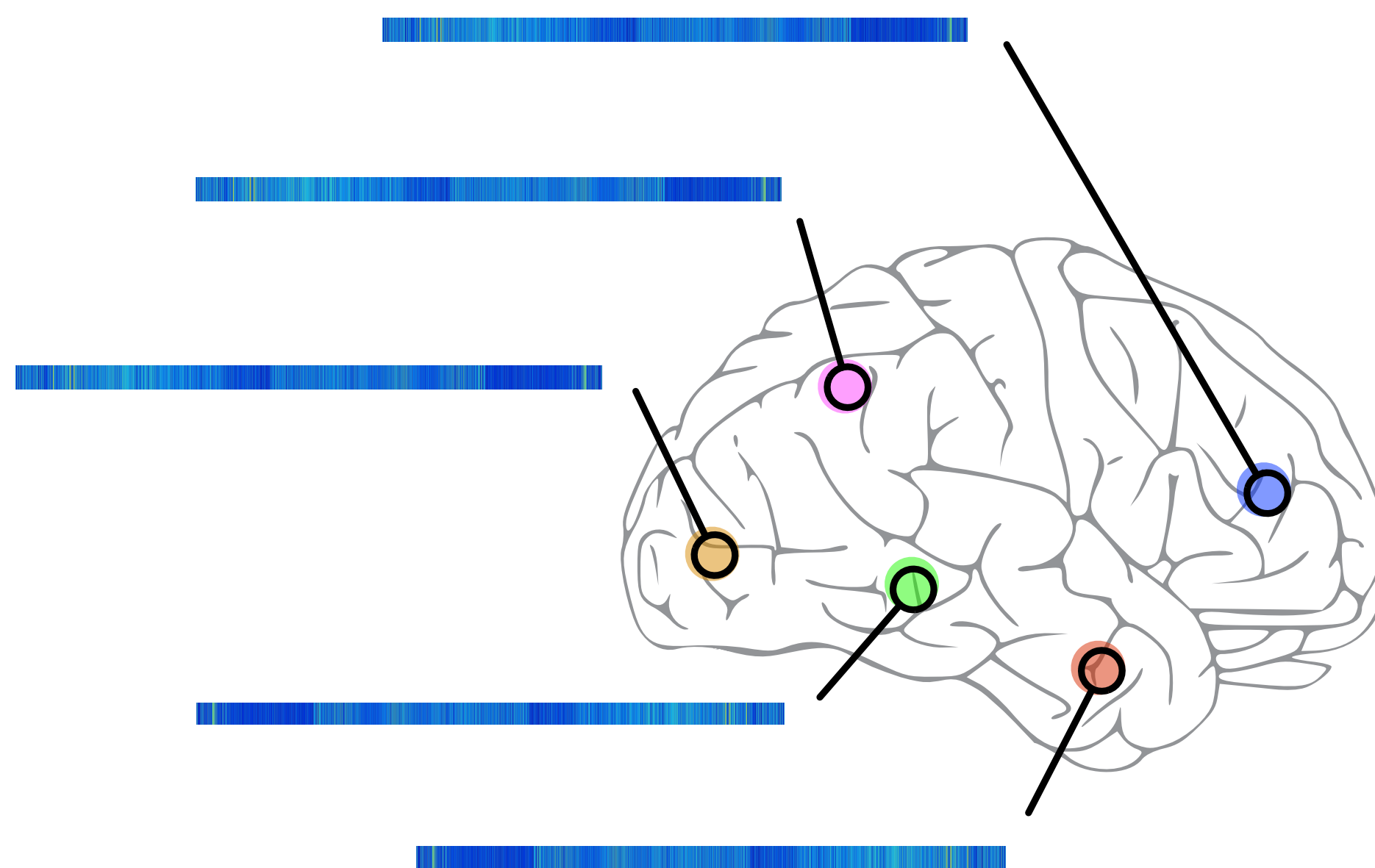
Functional networks genetics

fMRI data
(ICA-defined networks)



N=15, 18-29 y.o.
in vivo

Transcriptional similarity within functional networks

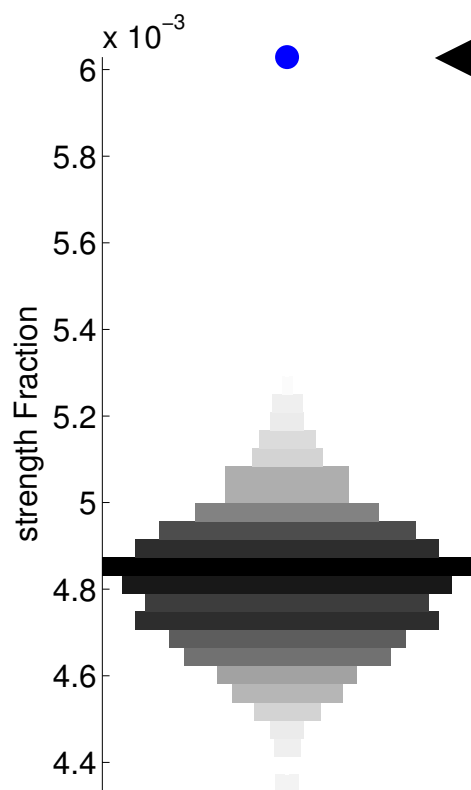


Gene expression per region

$$S_g = \frac{\sum_1}{\sum_{1+0} - \sum_1}$$

1 1 1 0 0

Regions grouped as belonging to FNs (1) or rest of brain (0)



← grouped by networks

← random groupings

p = 0.001

Holds with distance-corrected data, distance-preserving permutation

Genes driving the test

list overlap test + stability selection results

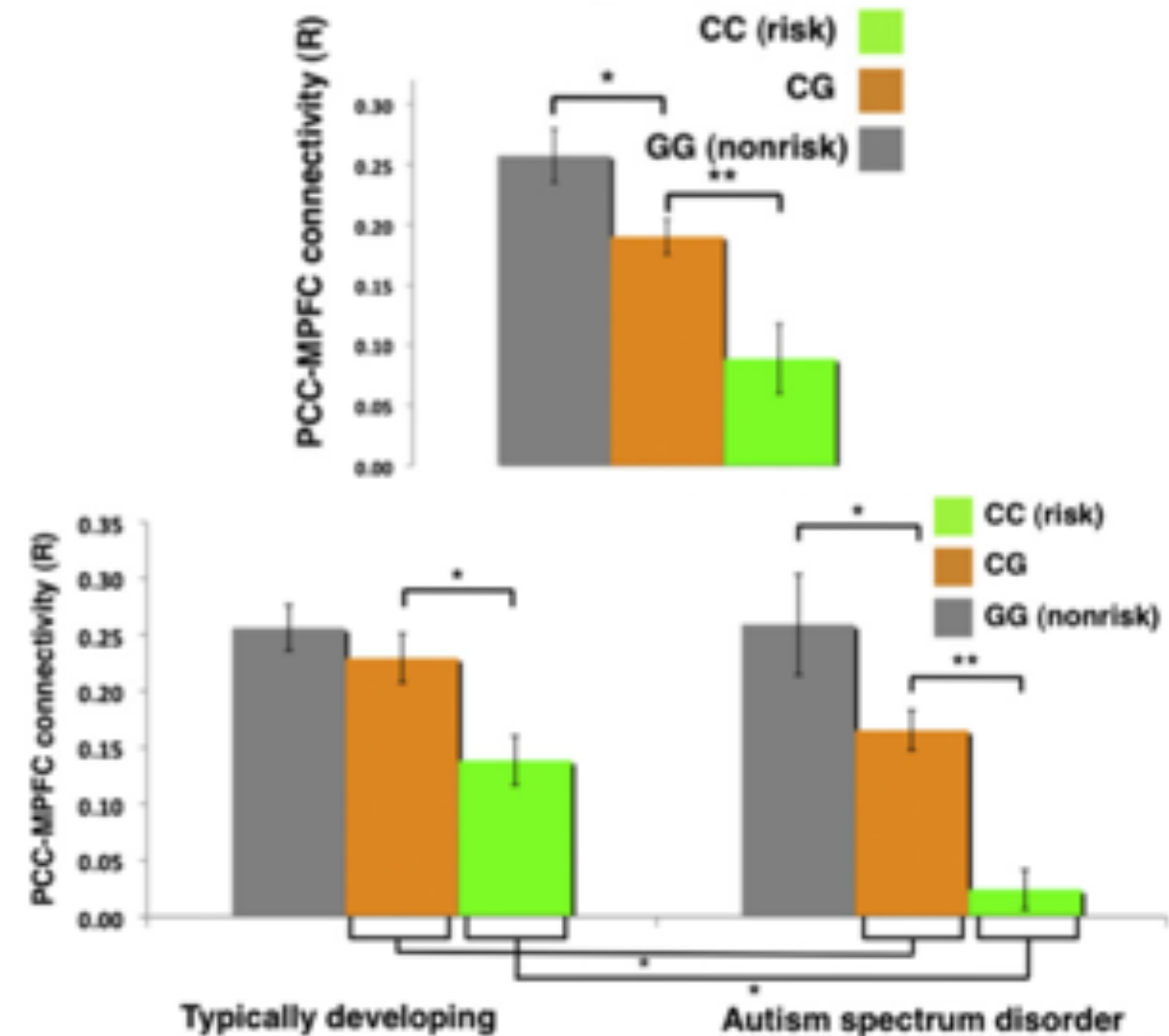
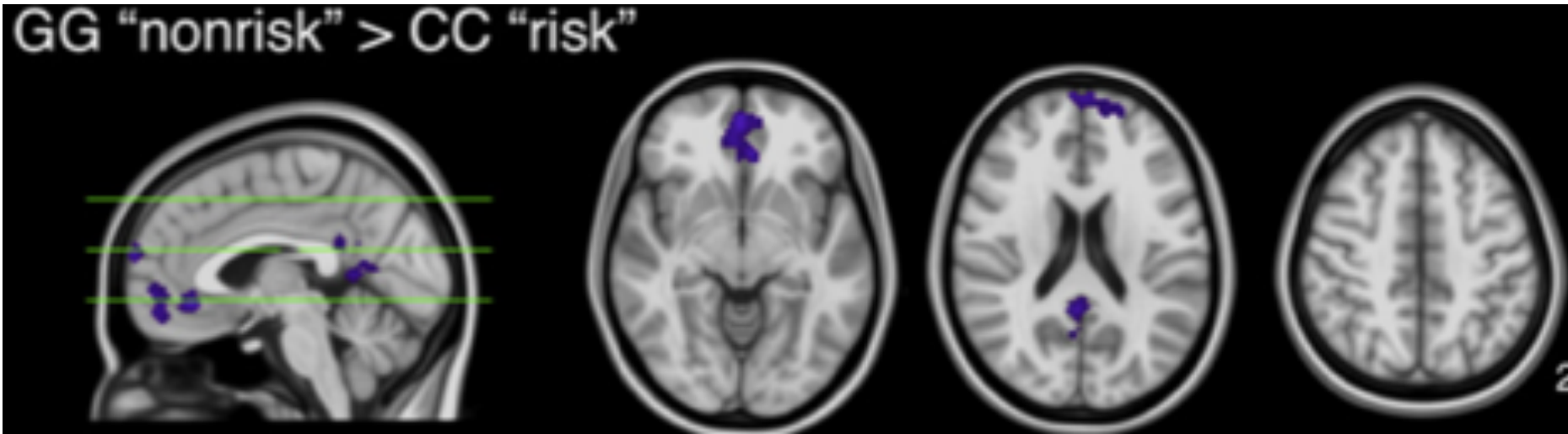
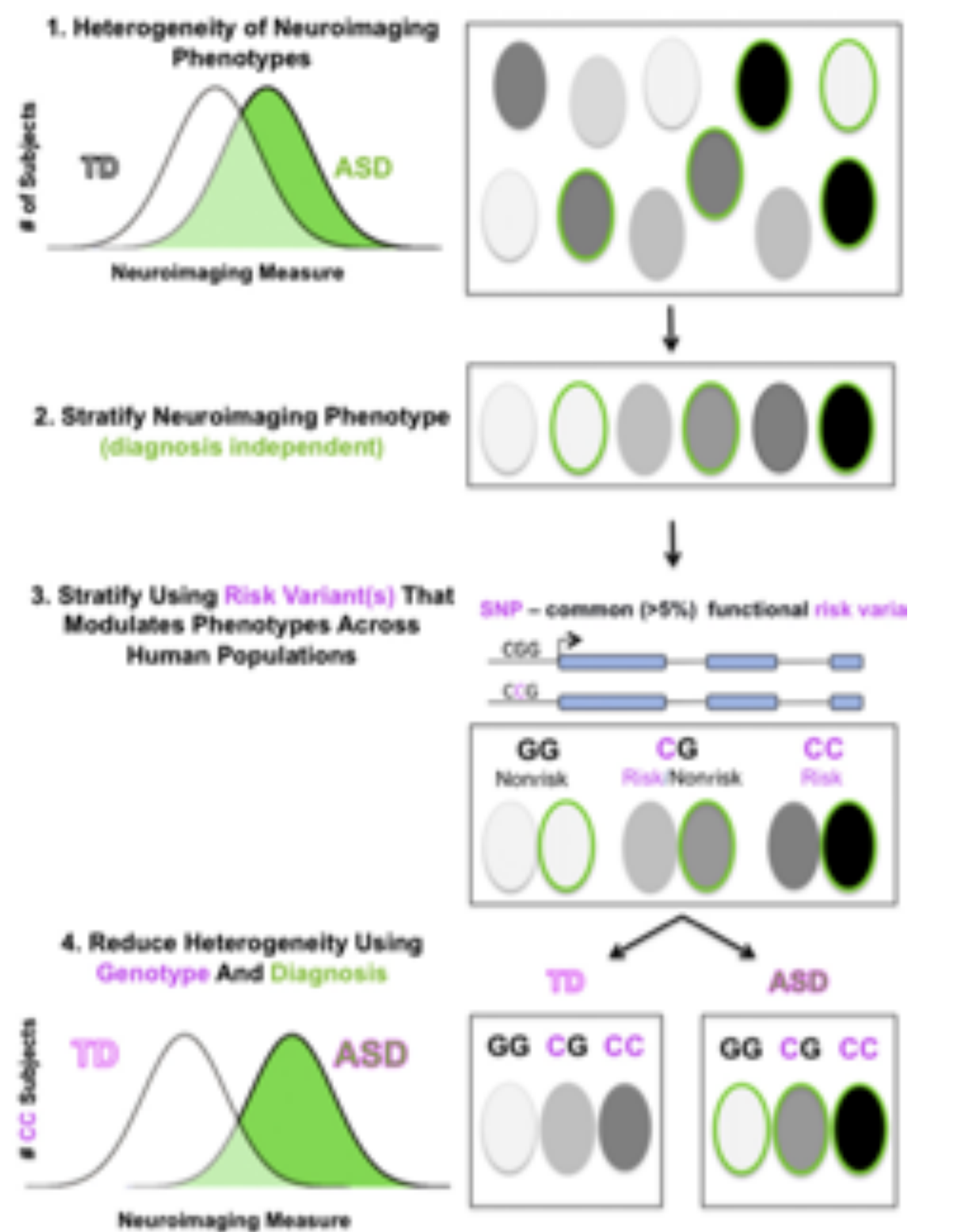
All splits (most stable)	ADAM23 ANKRD6 ATP6V1C2 BAIAP3 C3orf55 CARTPT CCDC39 CD70 CDK1 CNTN6 CRYBA2 CTXN3 CXXC11 DMRT3 EPN3 FEZF1 FZD7 GAL GLRA3 GNA14 GNGT2 GRP HSD11B1 KANK4 KCNA1 KCNA3 KCNA5 KCNC1 KCTD15 KRT1 KRT31 LAIR2 LINC00238 LMOD3 LRRC38 LYPLA2 MGP MYH7 MYLK3 NEB NECAB2 NEFH NEUROD6 NGFR NOL4 NOV NRP1 ONECUT2 PCP4 PIRT PNMT PRR15 PRSS35 PTGS1 RBP4 RBPMS2 RHOBTB2 RSPH9 SCARA5 SCN1B SCN4B SEMA7A SHD SHISA9 SIX3-AS1 SLC16A6 SLC22A10 SLN SV2C SYT10 SYT2 TDO2 TGFBI TINCR TLX2 TNNT2 TRIM29 TSHZ3	AMDHD1 ASGR2 CD163L1 COL5A2 CYP2C18 FAM163A GABRA5 GALP GPR26 GPR88 GPX3 HPCAL1 IL13RA2 ISCU NEXN NKAIN4 NPBWR2 ONECUT3 OR51E2 PLCH1 PVALB SNAP25 SPHKAP TMEM52 TSPAN8 ZCCHC18	5/6 splits
	ALOX12 CALB1 CCBE1 CD6 CDR2L CPLX1 ENPP6 GMPR GOLT1A GPR20 HOXD1 HPCA IL33 IQCJ KLK1 KLK8 LGR6 LINC00617 MS4A8 MYBPC1 NUPR1L PYDC1 RTP1 SEMA3C SH3RF2 SLC16A5 SLC20A2 SLC39A12 SOST WISP1 WISP2 WNT4	4/6 splits	

validated (n=259) in
association study using
SNPs of these genes with
in-vivo connectivity as
quantitative phenotype.

A few well-known genes like SNAP25 or GABRA5
Many potassium channels (KCN*)
Significant enrichment for voltage-gated ion channels

Brain network imaging genetics for stratification

MET genotype: CC lowers PCC↔MPFC conn



	CC	CG	GG	Σ
TD	9	15	9	33
ASD	7	24	7	38
Σ	16	39	16	71

Wrap-up and take-home points

Graphs offer an interpretable ‘meso-scale’ for medical image analysis, and a useful ‘inter-lingua’ between different modalities, organs, and biological scales

Graph estimation from medical imaging data can be improved from the status quo, yielding more desirable estimators

There has been tremendous progress over the past 10 years in graph analysis, particularly in scalable and predictive ML approaches

Graphs obtained from medical imaging, and their properties, can be used as a heritable and sensitive endophenotypes for genetic analyses

Thanks

Translational Machine Learning Lab



back Tommaso Di Noto**, Antoine Madrona, Xavier Sieber***,
Dr. Jonathan Patiño-Lopez, Jonas Richiardi
front Veronica Ravano*, *Dr Elda Fischi-Gomez*, Costa
Georgantas, Dr Jaume Banus Cobo, (Adrien Jammot)

Collaborators INRIA/CNRS/UGA

DrSc. Sophie Achard
Prof. JF Coeurjolly
Ms Hana Lbath

UNSW

Prof. P. Lafaye de Micheaux

BYU/UCSB

Prof. A. Petersen

UCL

DrSc Andre Altmann

Stanford

Prof. M. Greicius

CHUV/UNIL

DrSc Ruud van Heeswijk

Prof. Roger Hullin

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Dr Philippe Meyer

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